

Mobile Health

Lecture 4

Photoplethysmography (PPG) and Mobile Health (Part 2)

Cecilia Mascolo

PPG and Sleep

- Heart and respiration are indicative of different sleep stages.
- These, as we have seen, can be characterized with PPG.
- Also audio and movement differ in various phases of sleep (see upcoming audio lectures).



PSG: Sleep Monitoring Gold Standard

- Polysomnography (PSG) is a multi-sensor approach
 - electroencephalography (EEG),
 - electromyography (EMG)
 - electrooculography (EOG)
- Together facilitate the measurement of brain activity, alongside both muscle and eye movement.
- Measurements of respiratory and cardiac activity are also often included.

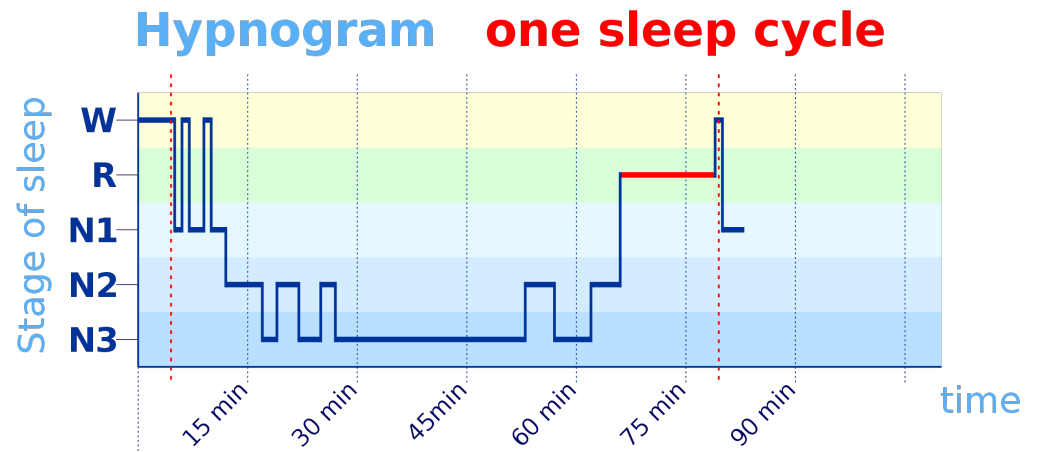


Alternatives...

- Basic measures of sleep eg duration, awake episodes, sleeping pattern, bedtime routine, perception after sleep.
- These could be asked through a questionnaire/sleep diary.
- Or
- Smartphones basic features:
 - Has the phone been used (when).
 - Accelerometer of phone placed on mattress can measure movements.
 - Microphone (for sleep apnea).
- Under mattress (acceleration/pressure).
- Contactless Radio (see upcoming lecture).

Sleep Epochs

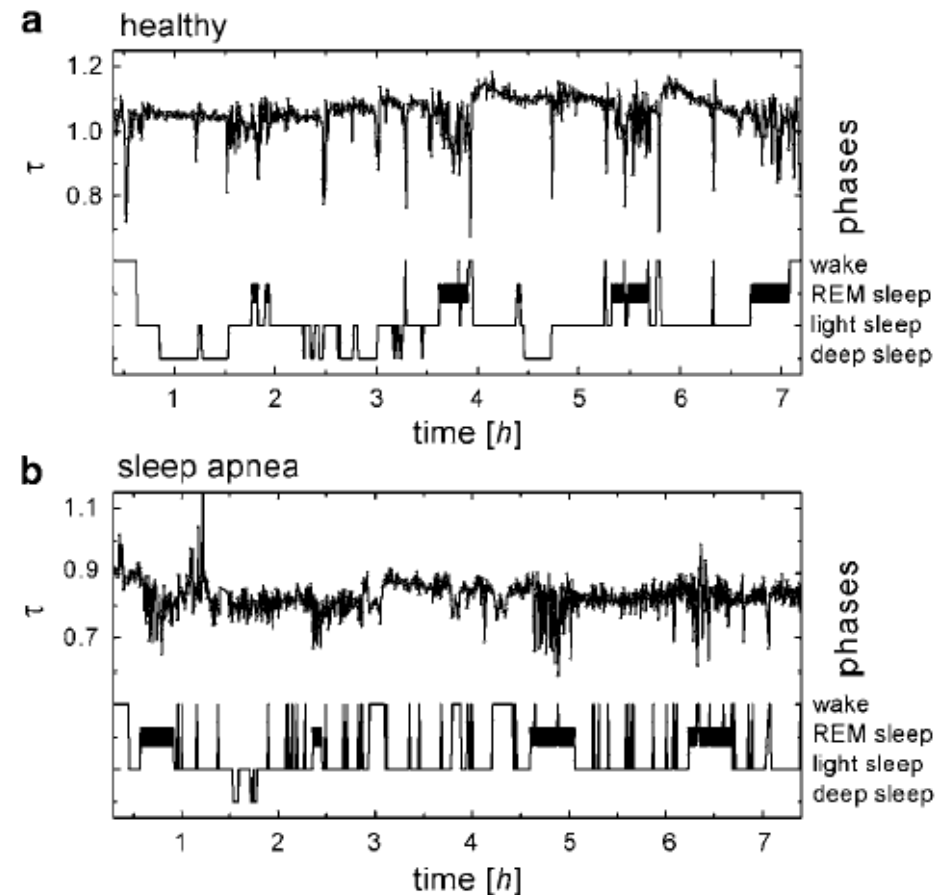
- There are up to six sleep stages:
 - awake;
 - rapid eye movement sleep (REM);
 - non-rapid eye movement (Non-REM);
 - sleep stage NREM 1 (N1);
 - sleep stage NREM 2 (N2);
 - sleep stage NREM 3 (N3).
- Each night has 4-6 cycles (90mins)



Sleep Apnea

- Sleep Apnea occurs when throat muscles relax and block air flow to the lungs.
- τ is a measure of IBI (inter beat interval)

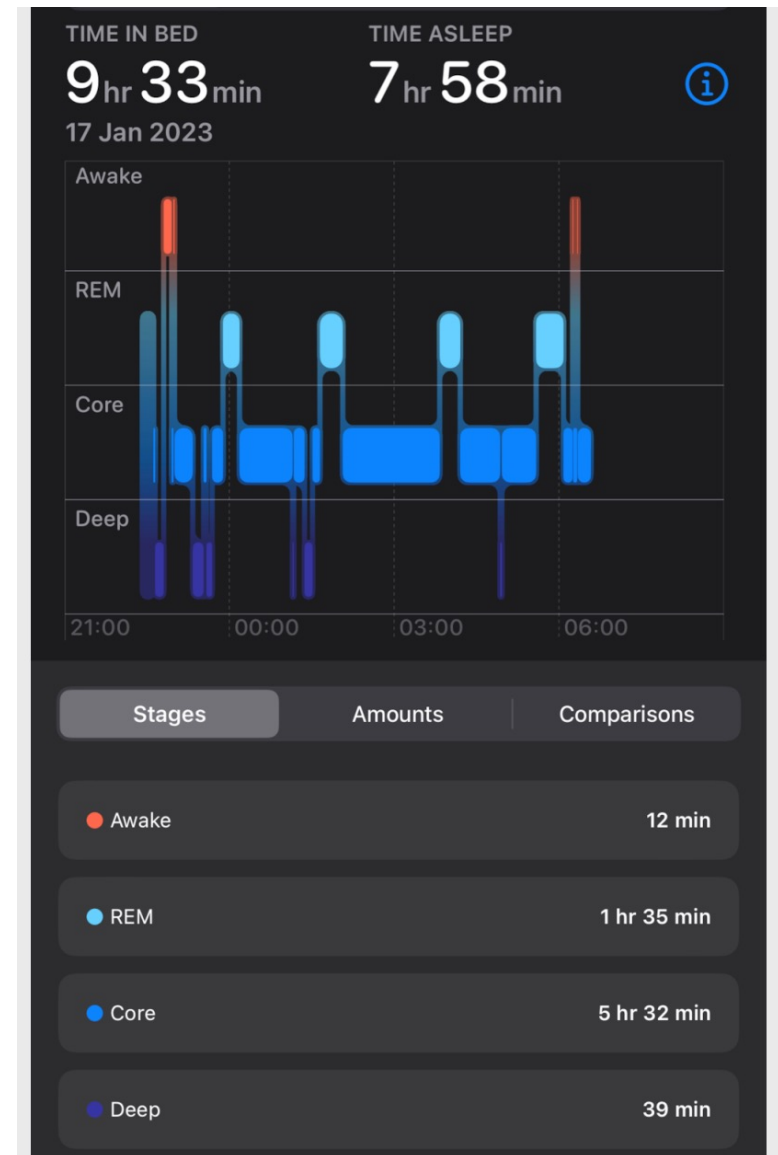
Y axis a measure of IBI



PPG!

- Wearables with accelerometers and PPG can measure motion as well as Heart Rate and PRW (pulse rate variability).
- PPG-based wearables identify wake and sleep with a performance similar to, or better than, research-grade actigraphy (accelerometer based) devices.
- Sleep stages monitoring is still accurate enough...

Sleep Tracking with PPG



PPG on wearables vs PSG

Wearable	n	PSG					SE
		TST	Light sleep	Deep sleep	REM sleep	WASO	
Mi Band2	55	r = 0.367 ** ICC = 0.297*	r = 0.032 ICC = 0.024	r = 0.116 ICC = 0.095		r = 0.383 ** ICC = 0.148	
Gear Fit2	54	r = 0.307 * ICC = 0.209					r = 0.18 ICC = 0.048
Fitbit Alta HR	61	r = 0.466 *** ICC = 0.205	r = 0.179 ICC = -0.19	r = 0.372 ** ICC = 0.301 **	r = 0.310 * ICC = 0.323 **	r = 0.425 *** ICC = 0.213 *	

Light sleep: sum of N1 and N2 sleep

Deep sleep: N3 sleep

TST: Total sleep time

REM: Rapid eye movement

WASO: Wake time after sleep onset

SE: Sleep efficiency

r: Spearman's rho

ICC: Intraclass correlation coefficient

* $p < 0.05$, ** $p \leq 0.01$, *** $p \leq 0.001$

The deep sleep duration, REM sleep duration, and WASO measured by the Fitbit Alta HR significantly correlated with PSG results, although Fitbit Alta HR underestimated the duration of light sleep when compared to PSG (253 min vs 287 min).

Kim, K., Park, D.Y., Song, Y.J. *et al.* Consumer-grade sleep trackers are still not up to par compared to polysomnography. *Sleep Breath* 26, 1573–1582 (2022).

How do we calculate Sleep Stages from PPG?

An example

- Sleep epochs of 30s.
- Motion features
 - Activity count over epoch (e.g. integrated area under the accelerometer signal).
 - Accelerometer magnitude.
 - Time since last significant movement.
 - Time till next significant movement.

Estimation of sleep stages in a healthy adult population from optical plethysmography and accelerometer signals. Z Beattie, Y Oyang, A Statan, A Ghoreyshi, A Pantelopoulos, A Russell and C Heneghan.. 2017 Institute of Physics and Engineering in Medicine Physiological Measurement, Volume 38, Number 11.

Examples of patterns vs sleep stages

- An activity count feature which includes the magnitude and duration of movement during the 30 s epoch is easily interpreted as being correlated with wake.
- Periods of near-constant heart rate and low movement are associated with deep sleep.
- Periods with a high degree of short-term heart rate variability (e.g. as seen in the LF and HF spectral features) and relatively little movement are associated with REM.

Heart Rate Variability Features

- Inter Beat Interval to calculate Heart Rate Variability:
 - High Frequency (eg through DFT) 0.15–0.4 Hz
 - Low Frequency 0.04–0.15 Hz
 - VLF power (0.015–0.04 Hz)
 - RMSSD: Root mean square of successive differences of IBI
 - pNN50: proportion of successive IBIs that differ more than 50ms over total IBIs
 - Delta IBIs
 - Mean heart rate
 - 90th percentile heart rate
 - 10th percentile heart rate

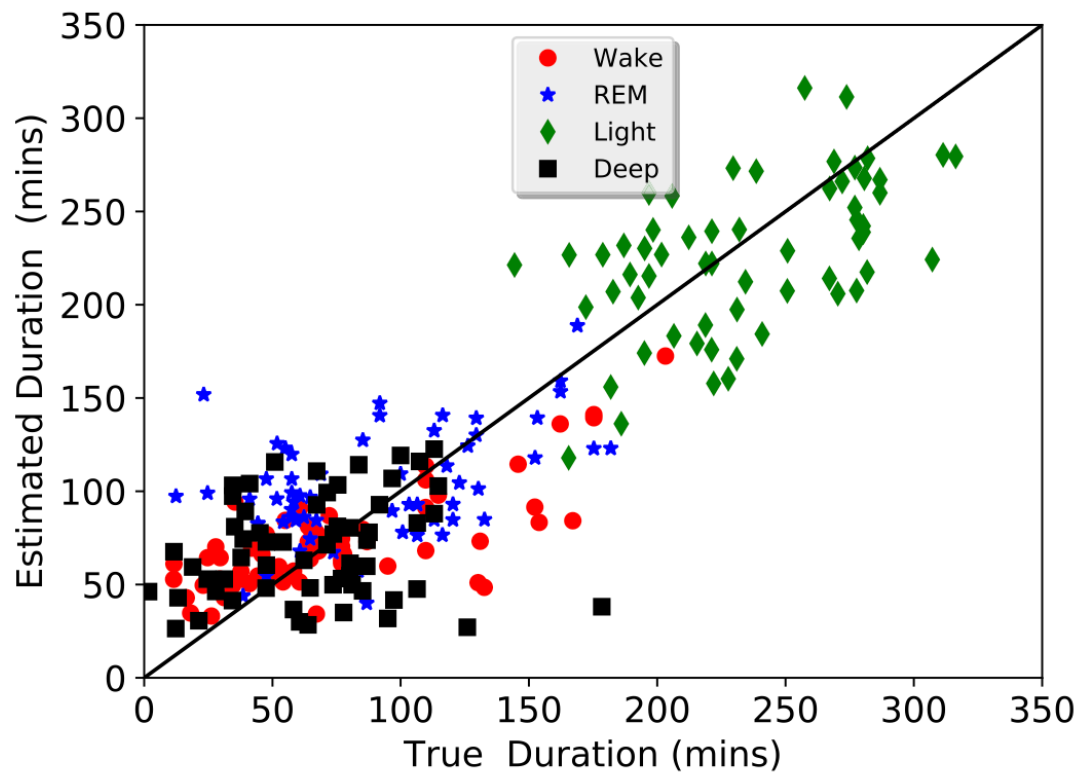
Breathing Features (see previous lecture)

1s breathing sample: take the frequency spectrum (and limit the power of frequency to plausible breathing frequencies).

- HF power (0.15–0.4 Hz)
- LF power (0.04–0.15 Hz)
- VLF power (0.015–0.04 Hz)

Results

	Predicted stage				
	Wake	REM	Light	Deep	
Actual (%) stage	Wake (15.7%)	6116	640	2035	33
	REM (19.1%)	424	7653	2566	47
	Light (50.8%)	1995	3598	19681	3179
	Deep (14.4%)	145	314	2583	5056



Results

Parameter	Percentage
Overall sensitivity (in detecting sleep)	94.6
Specificity (in detecting wake)	69.3
PSG-tracker agreement (light sleep)	69.2
PSG-tracker agreement (deep sleep)	62.4
PSG-tracker agreement (REM sleep)	71.6

Cohen's Kappa is used to rate agreement between
PSG and tracker

$$\kappa = \frac{\% \text{Observed Agreements} - \% \text{Agreements by chance}}{1 - \% \text{Agreements by chance}}.$$

New wearables and sleep...

- Oura Ring
- Oura underestimated TST and overestimated WASO.
- Oura significantly underestimated REM sleep and light sleep (stage N1+N2), and overestimated time spent in deep sleep (stage N3)



[Nat Sci Sleep](#). 2021; 13: 177–190.

Published online 2021 Feb 15. doi: [10.2147/NSS.S286070](https://doi.org/10.2147/NSS.S286070)

PMCID: PMC7894804

PMID: [33623459](https://pubmed.ncbi.nlm.nih.gov/33623459/)

Multi-Night Validation of a Sleep Tracking Ring in Adolescents Compared with a Research Actigraph and Polysomnography

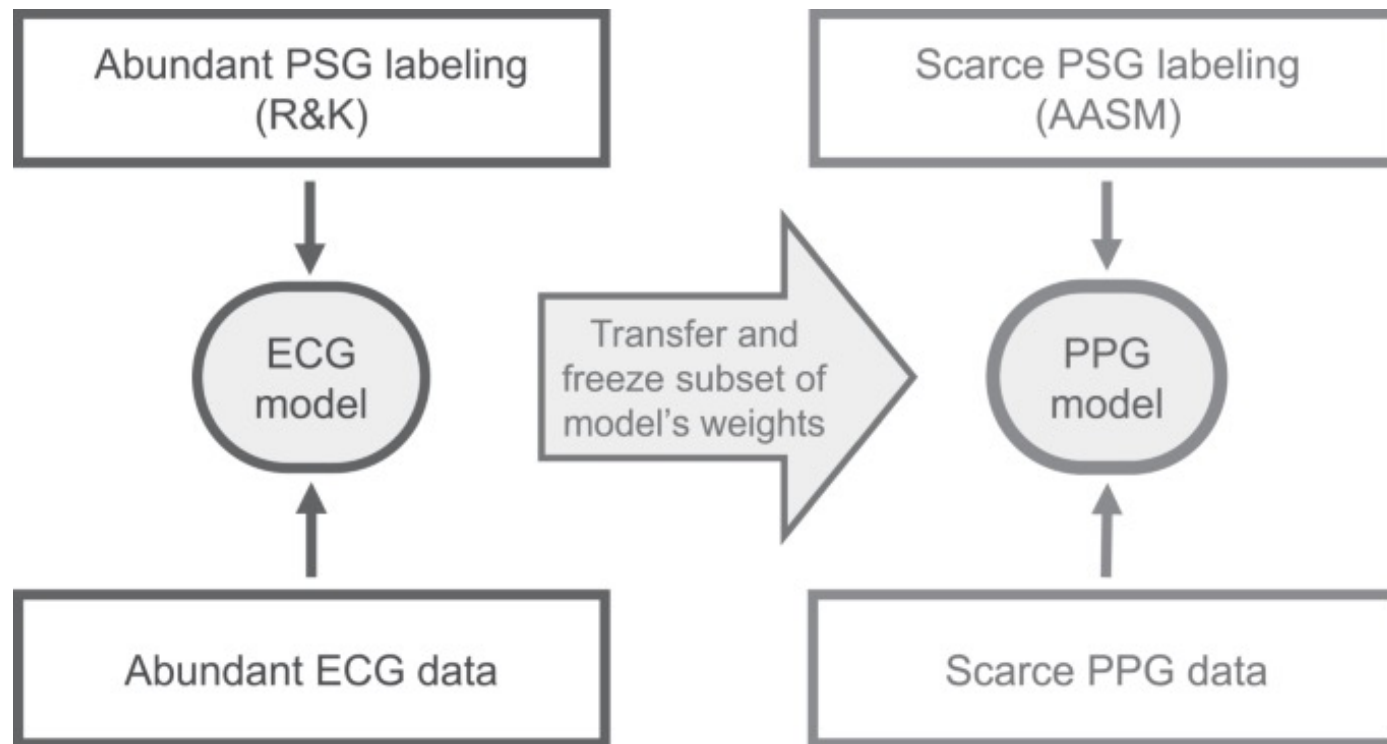
[Nicholas I Y N Chee](#),^{#1,*} [Shohreh Ghorbani](#),^{#1,*} [Hosein Aghayan Golkashani](#),¹ [Ruth L F Leong](#),¹ [Ju Lynn Ong](#),¹ and [Michael W L Chee](#)¹



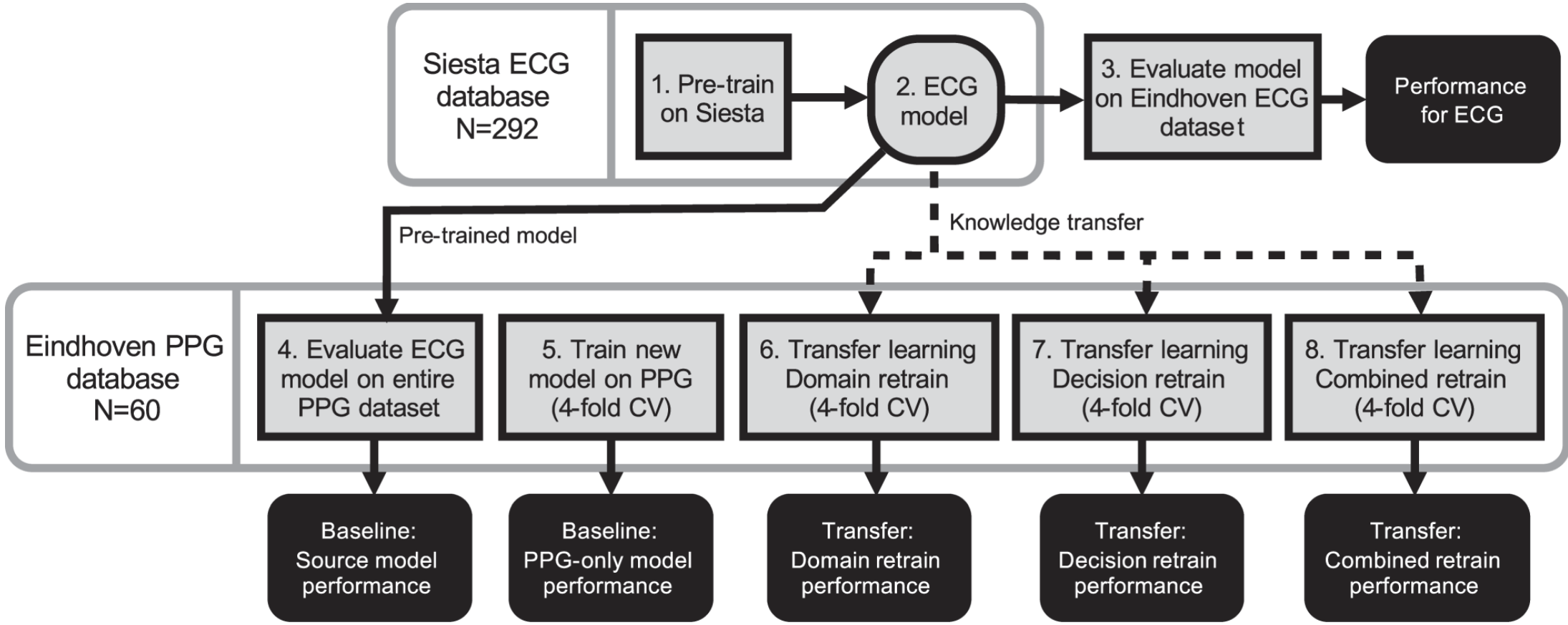
Deep Learning approaches over PPG Sleep

- Works that use **transfer learning**: model trained on a large database of heart rate variability (HRV) measures and then fine-tuned to a smaller database of pulse rate variability (PRV) measures derived from the IBIs detected on the PPG.
- ECG can be used to calculate HRV and HRV can be correlated with sleep stages (LSTM models seem good)
- There is a lot of ECG data: train on that!
- Then transfer to lower data regime.

Deep learning approaches over PPG Sleep

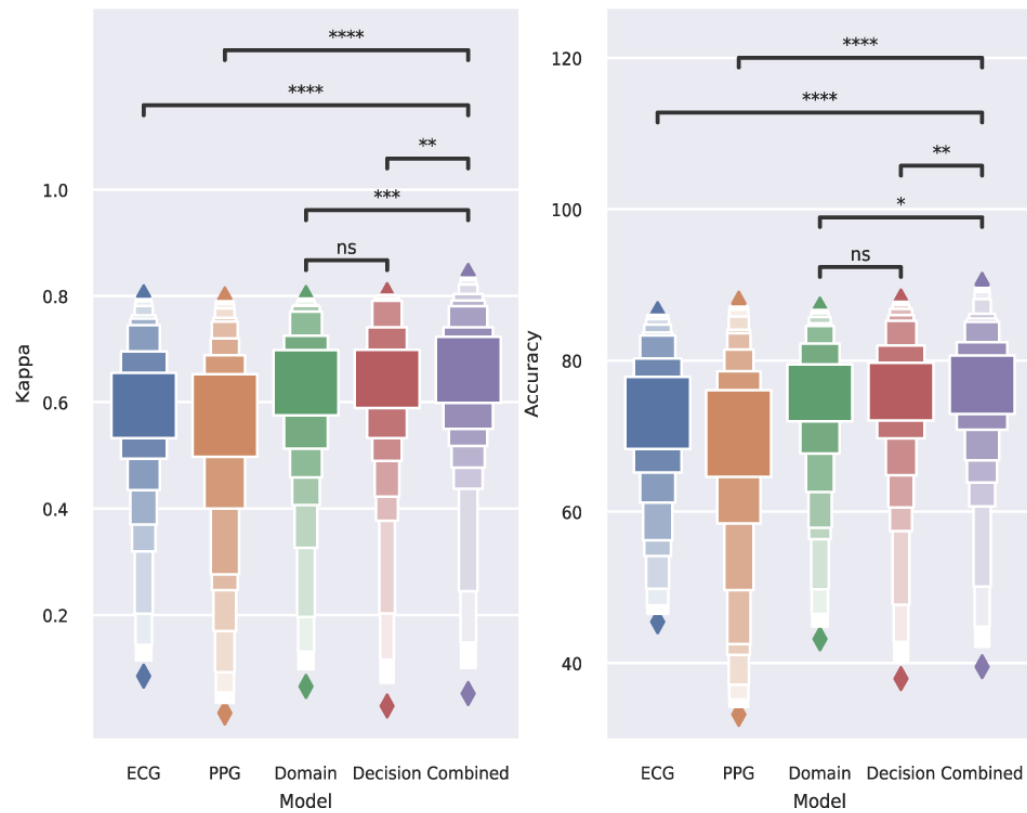


Radha, M., Fonseca, P., Moreau, A. et al. A deep transfer learning approach for wearable sleep stage classification with photoplethysmography. *npj Digit. Med.* 4, 135 (2021).

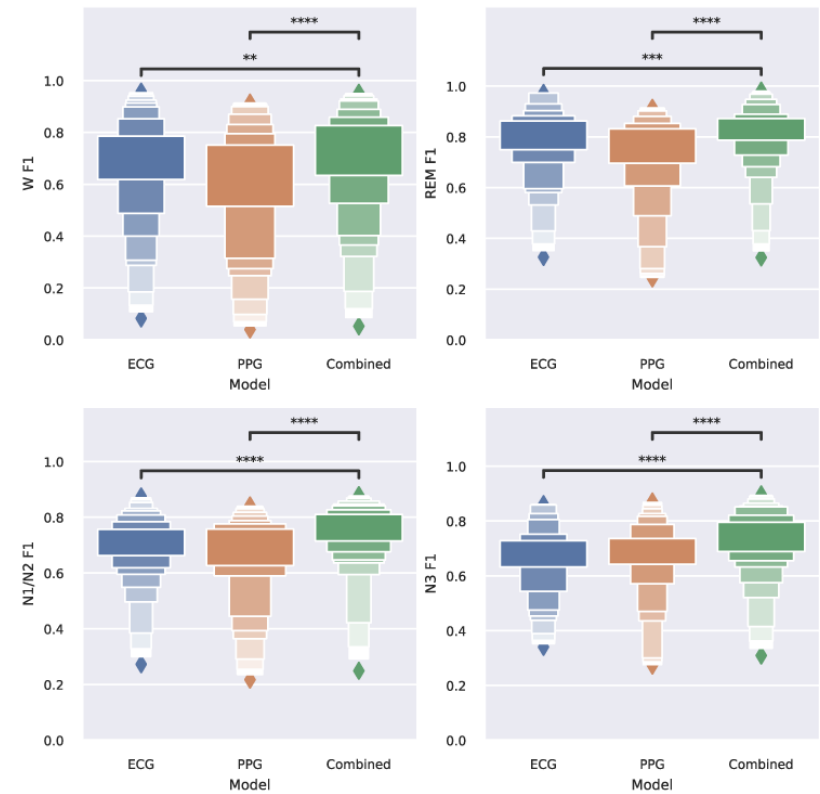


Performance

a



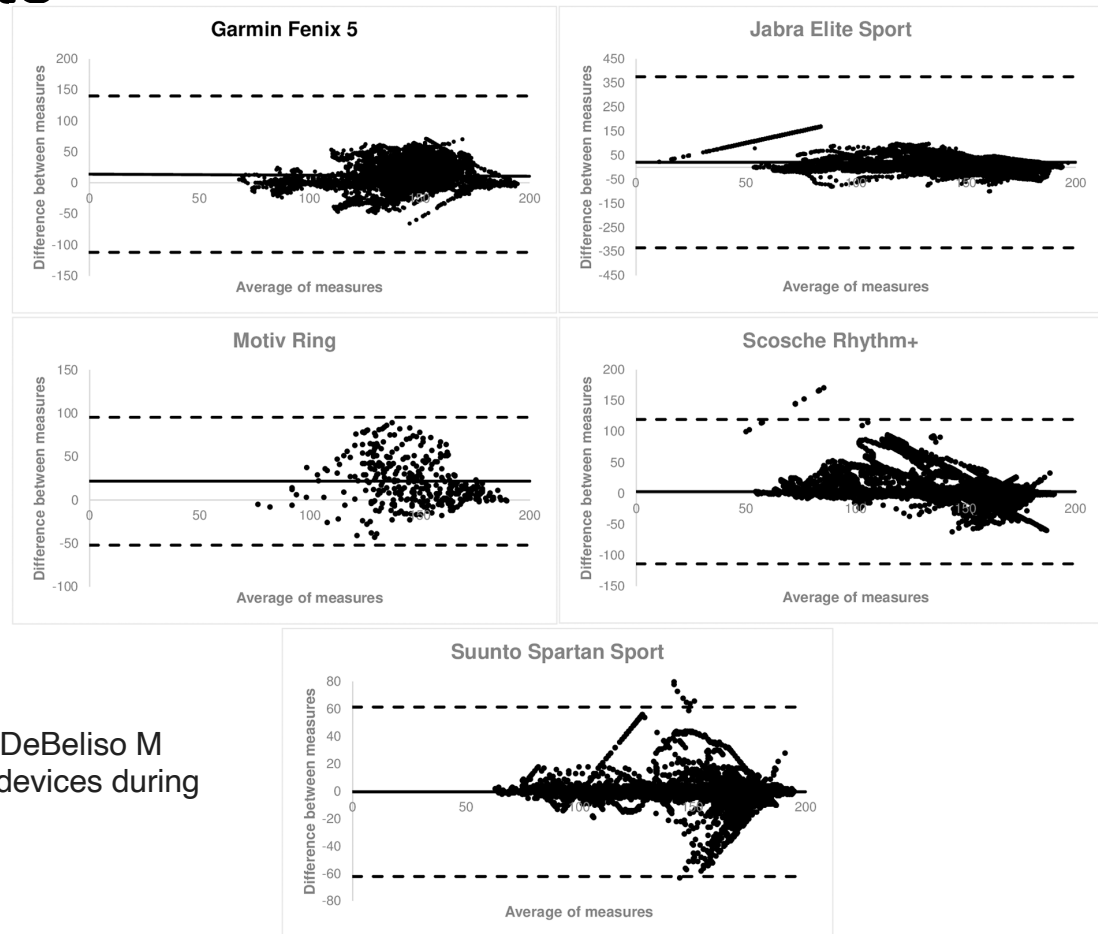
b



PPG. When does it not work: Motion... Bland-Altman Plots

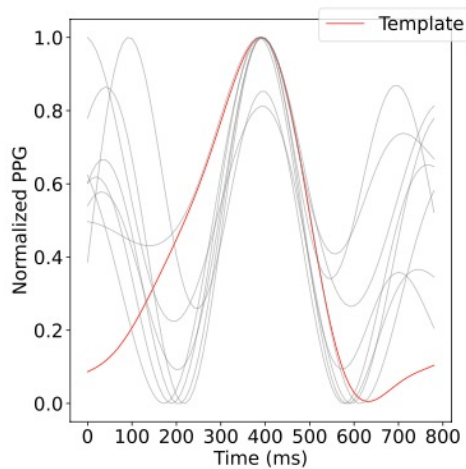
Polar 7 strap as ground truth

Heart Rate Measures

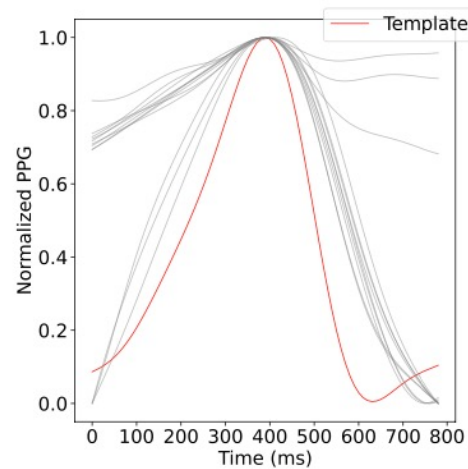


Navalta JW, Montes J, Bodell NG, Salatto RW, Manning JW, DeBeliso M (2020) Concurrent heart rate validity of wearable technology devices during trail running. PLoS ONE 15(8).

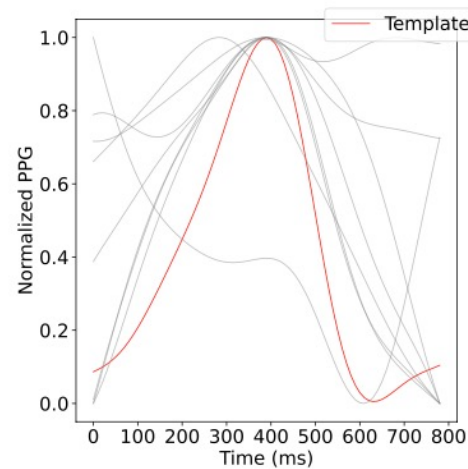
PPG on Earables. When does it not work: Micro motion...



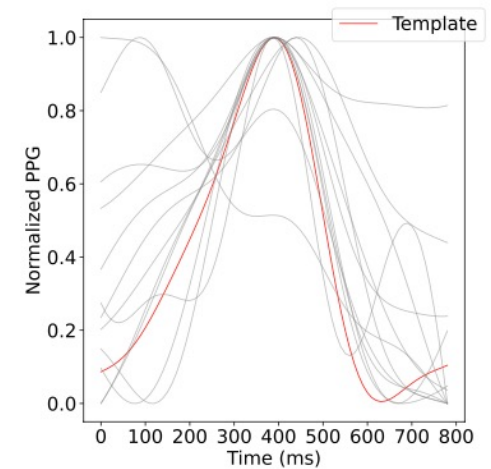
(a) Shake.



(b) Brow Raiser.



(c) Lip Puller.



(d) Mouth Stretch.

Red line: PPG in stationary case. Gray line:(same user) in various motion sessions for that movement

PPG. When it does not work: Skin colour

- Paper [1] discusses:
 - That Paper [2] found no significant difference in accuracy across skin tones but did find differences by devices in response to changes in activity.
 - Previously reported studies [3] finding wearables using green light technology had larger errors rates in tracking heart rate and energy expenditure for individuals with darker skin tones especially if exercising.
 - Racial biases and limitations of Fitzpatrick Skin Type Scale: originally used for propensity skin to burn :)
 - Too few people with the darkest skin tones were included ($n = 9$ in FST Type 6) in paper [2].

References on the next slide.

References from previous page

[1] Colvonen, P.J. Response To: Investigating sources of inaccuracy in wearable optical heart rate sensors. *npj Digit. Med.* 4, 38 (2021).

[2] Bent, B., Goldstein, B.A., Kibbe, W.A. *et al.* Investigating sources of inaccuracy in wearable optical heart rate sensors. *npj Digit. Med.* **3**, 18 (2020).

[2] Shcherbina A, Mattsson CM, Waggott D, Salisbury H, Christle JW, Hastie T, Wheeler MT, Ashley EA. Accuracy in Wrist-Worn, Sensor-Based Measurements of Heart Rate and Energy Expenditure in a Diverse Cohort. *J Pers Med.* 2017 May 24;7(2):3.

Expert insight into current research

News & views

Racism in science

Forum: Medical devices

Skin colour affects oxygen-sensor accuracy

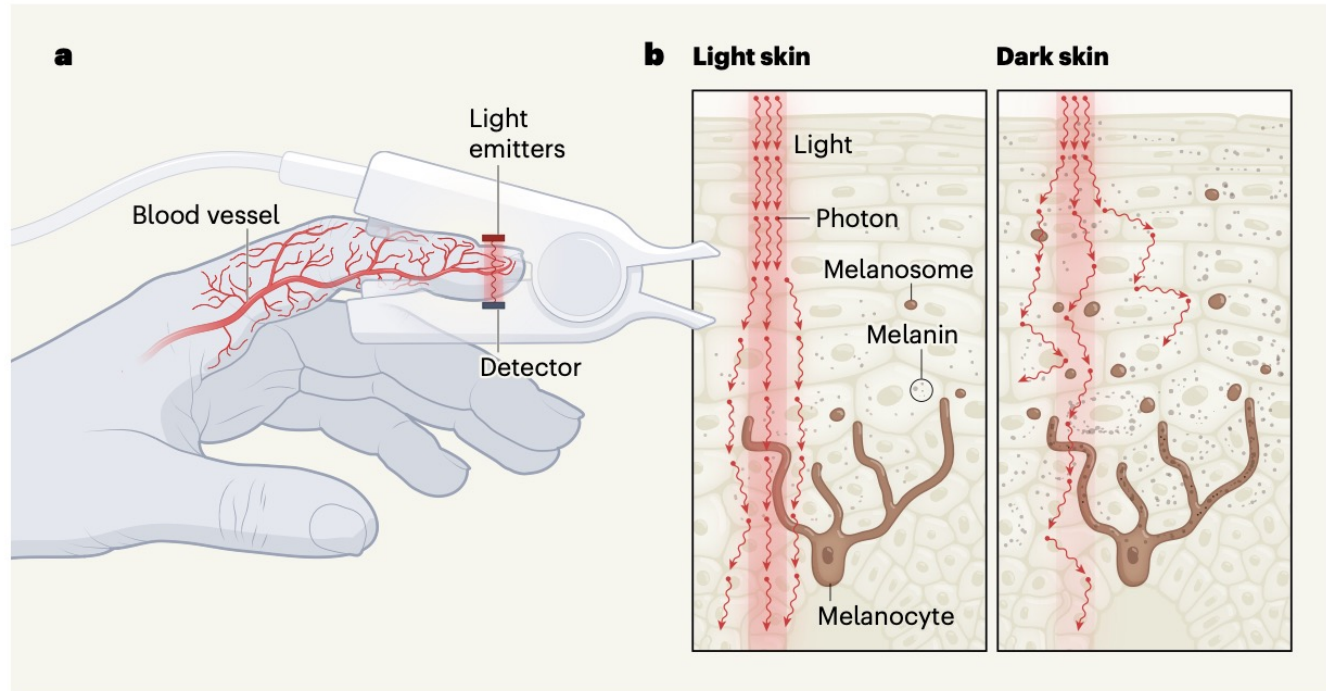
COVID-19 broadened the use of pulse oximeters for rapid blood-oxygen readings, but it also highlighted the fact that skin pigmentation alters measurements. Two groups of researchers analyse this issue, and its effects on people with dark skin.

**Matthew D. Keller
& Brandon Harrison-Smith**
Pulse-oximetry errors affect patient outcomes

Since Sjoding and colleagues' report, several large retrospective studies have confirmed that darker-skinned people (those self-identifying as Black, Asian, Hispanic or a combination of these) are more likely than white people to experience occult hypoxaemia²⁻⁵. In one study of people with COVID-19,

had equivalent arterial blood-gas values³. A more comprehensive analysis showed that, even when baseline health conditions are taken into account, people with occult hypoxaemia are prone to organ dysfunction and in-hospital mortality, and that Black people in this group have the worst organ dysfunction⁵.

Although clinical reports of skin-colour bias in pulse oximetry were not widespread until the COVID-19 pandemic, evidence for this issue has been accumulating for decades^{6,7}. A comparison reported in February found that pulse-oximeter readings from nine devices were consistently less accurate for darker-skinned people than for lighter-skinned people⁸. But the study also found that testing healthy individuals under carefully controlled laboratory conditions resulted in fewer cases of occult hypoxaemia than are measured in hospitals. In fact, none of the 491 people who were tested by the authors had readings consistent with occult hypoxaemia, whereas Sjoding and colleagues tallied 187 cases out of 3,527 measurements from a



Nature 610, 449-451 (2022)

Figure 1 | Pulse-oximetry accuracy varies with skin tone. **a**, Devices known as pulse oximeters estimate the oxygen concentration in a person's blood by shining red and infrared light through their fingertip. Oxygenated haemoglobin absorbs infrared light more efficiently than it does red light, whereas the opposite is true for deoxygenated haemoglobin. **b**, These signals are affected by melanin, which is distributed through the skin in structures, known as melanosomes, that are produced by cells called melanocytes. Melanosomes in dark skin are both larger and more numerous than are those in light skin. Long-standing oximetry theory does not fully account for the way in which photons are scattered by the biomolecular content and structure of the tissue, and thus imprecisely corrects for the effect of pigmentation. Calibration studies compound this problem, because they typically oversample light-skinned people. This has led to overestimation of the oxygen concentration in some Black individuals' blood, and therefore to missed diagnoses of dangerously low oxygen levels.

Questions