

# Mobile Health

## Lecture 5

# Audio Signal and Health

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# An Affordable Sensor



# Automated Sound based Diagnostics



# Voice-based Diagnostics

**MIT  
Technology  
Review**

Artificial Intelligence / Machine Learning

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## Voice Analysis Tech Could Diagnose Disease

Researchers enlist smartphones and machine learning to find vocal patterns that might signal post-traumatic stress disorder or even heart disease.

by **Emily Mullin**

Jan 19, 2017

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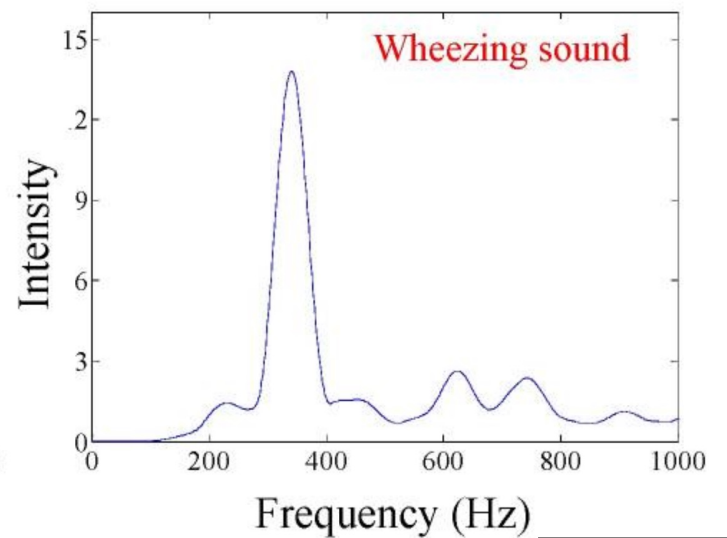
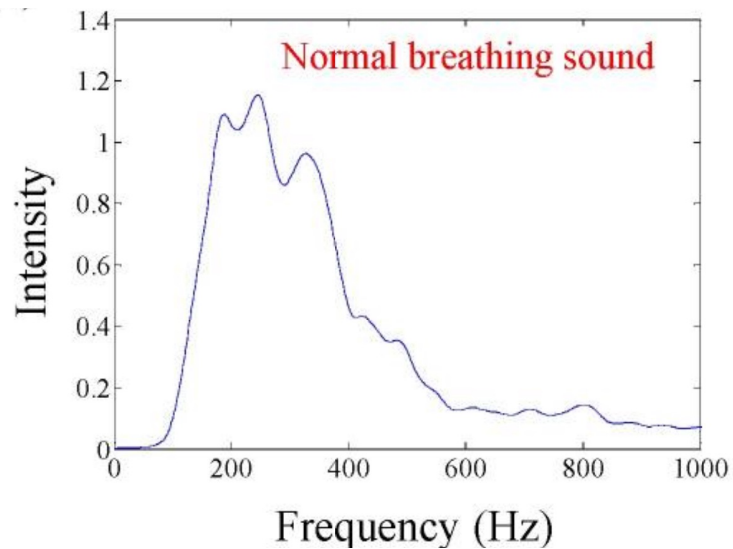


# Type of diseases for which audio has been tried on

- Depression and PTSD
- Sleep Apnea
- Wheezing (Asthma)
- Parkinson's
- Alzheimer's
- Autism
- Cardiovascular: coronary heart disease, arteriosclerosis
- ...

# Wheezing Detection

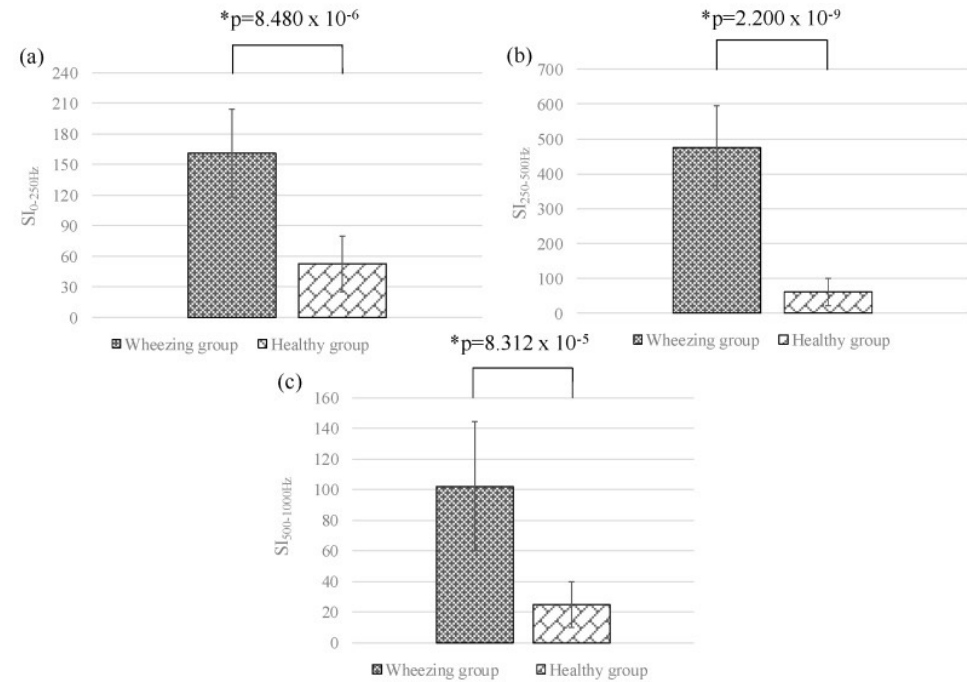
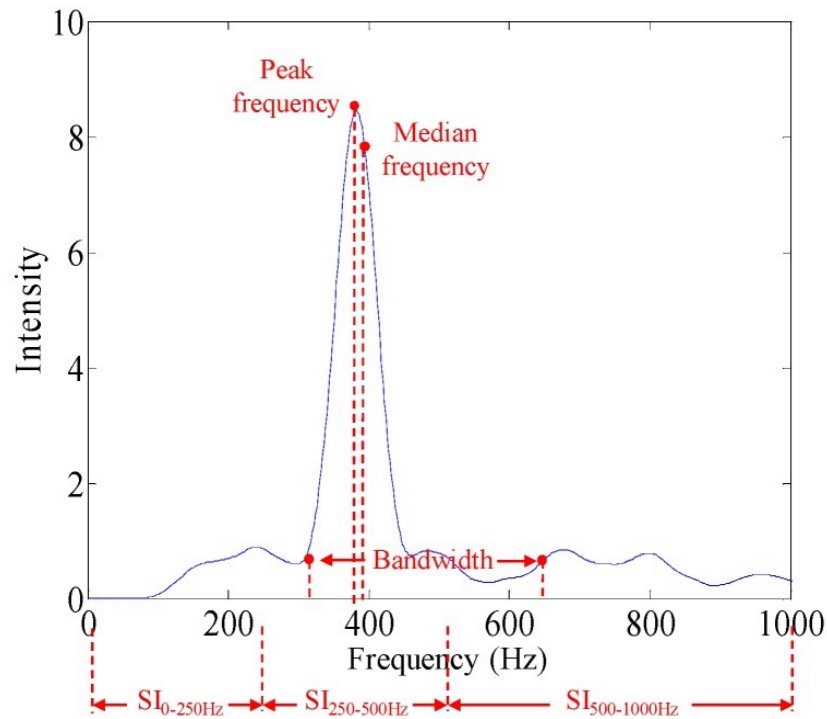
- Wheezing sound is a continuously abnormal breathing sound



# Preprocessing of this signal

- Band pass filter applied: (150 Hz–1000 Hz)
  - Cut out heart sound, muscle and blood interference sound.
- Raw breathing sound split into 250-ms breathing sound segments with 200-ms overlapping.
- Power spectrums of these breathing sound segments calculated by using DFT with a Hann window.

# Wheezing Features





# Important Features

ASE= audio spectral envelope

TI = tonal index

CF1= correlation feature

ER = Energy ratio

K= Kurtosis, Difference to mean ratio

EVD = Eigen Value Decomposition

VC = Vector Comparison

LP = Linear prediction

SPE = Spectral peak entropy

SF = Spectral flatness

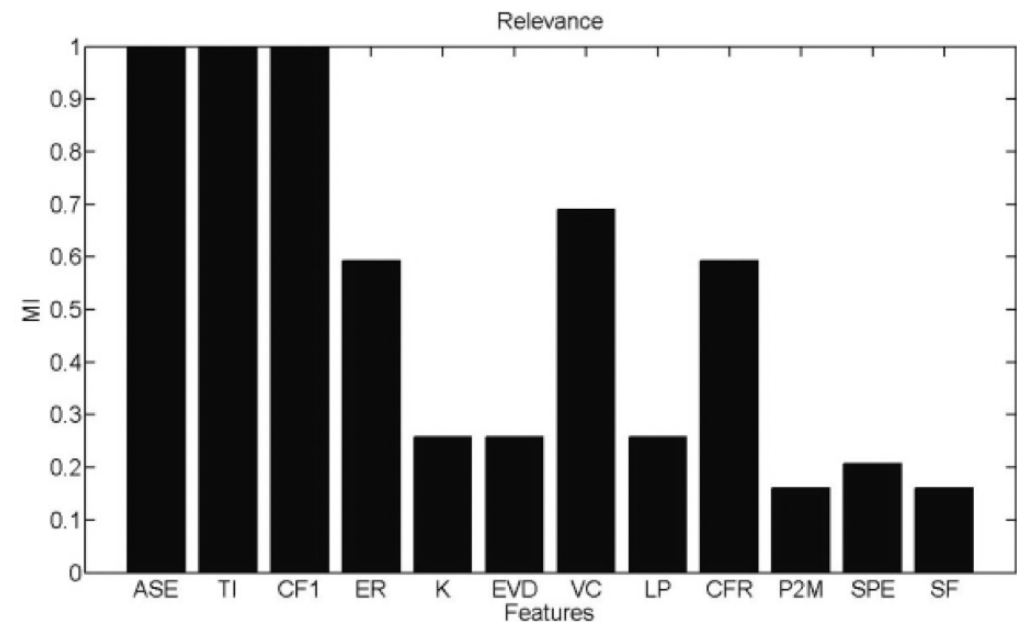
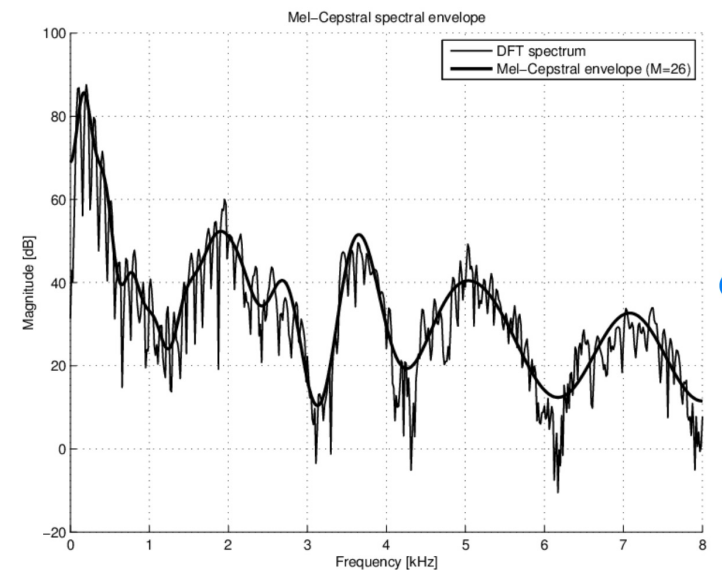


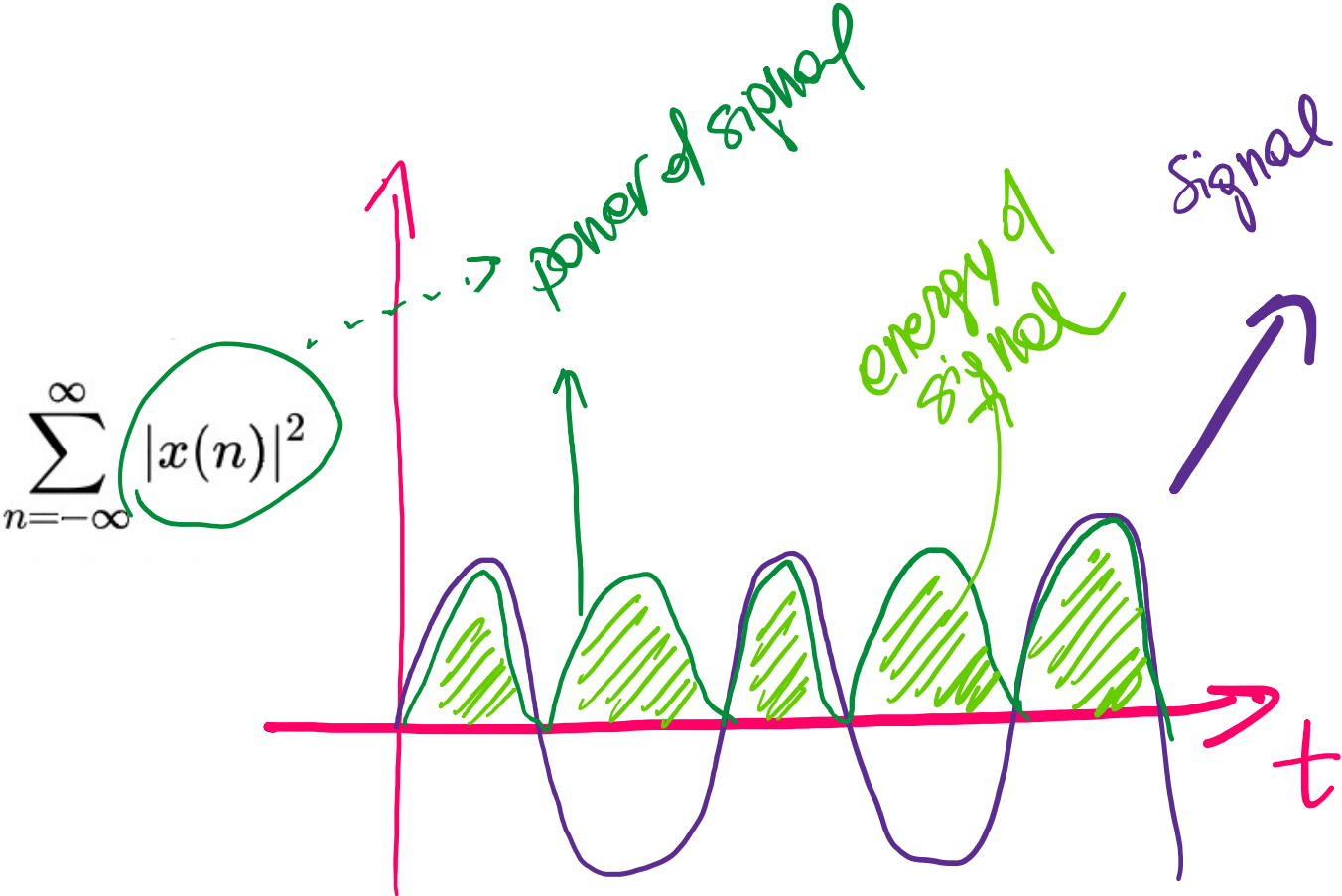
Fig. 2. Relevance of the tested features calculated for real lung recordings using the mRMR algorithm

# Frequency Spectrum Envelope

- Identifies the max frequency of each frame and creates a curve which represents all those maximum frequencies.
- Sometimes the frequency spectrum is “smoothened” first.



# Energy of the Signal



# Linear Prediction Coefficients

Technique that calculates coefficients of a linear prediction model which predicts the next sample of audio from a sequence of  $k$  previous samples. The coefficient of this linear model are those coefficients. This technique is used to predict **pitch period** accurately (ie the period at which a signal pattern repeats).

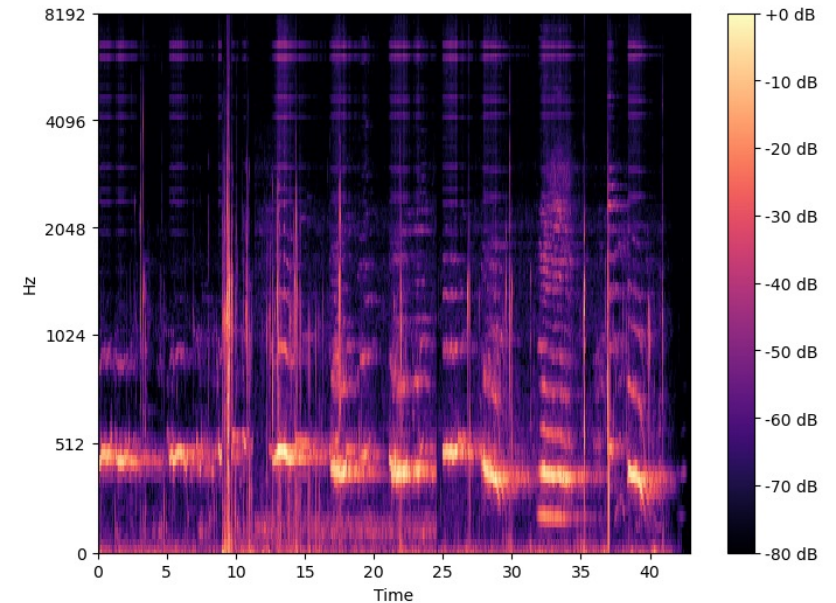
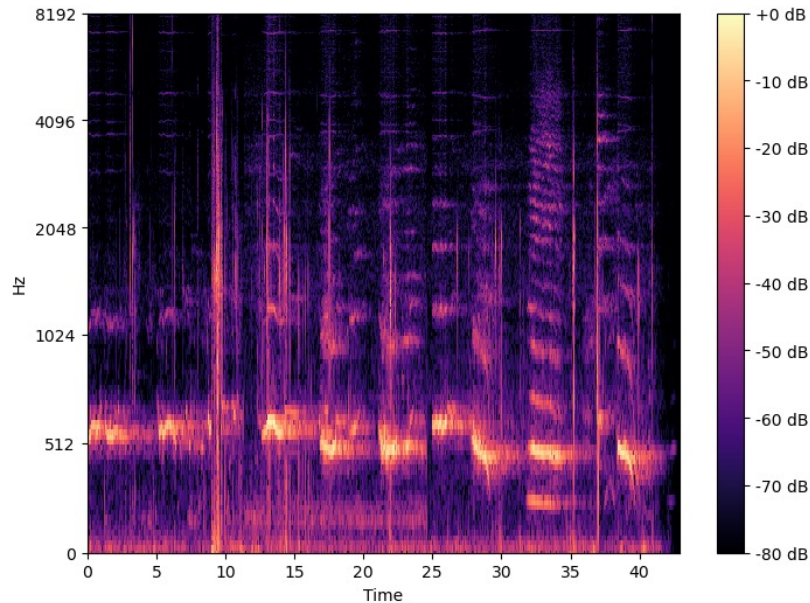
# MFCCs (Mel-frequency cepstral coefficients) Features

- Very used in audio processing
- The intuitively match our auditory way of perceiving sounds

# From Spectrograms to Mel Spectrogram

- Spectrogram 1 is the output of standard DFTs.
- However humans perceive frequency of sound “logarithmically”
  - Difference between sounds at lower frequency seems more than difference of sounds at higher frequency

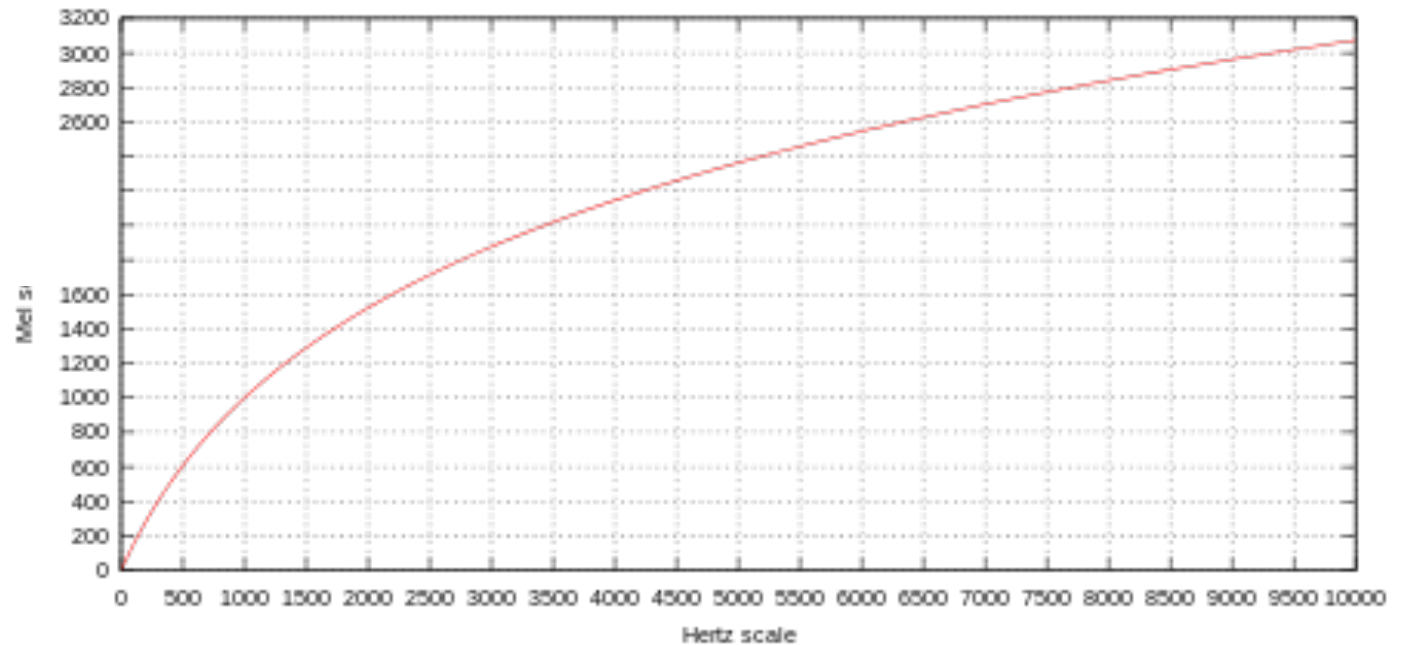
Whale song 😊



# Mel Scale

- Mel Scale is perceptually relevant scale for frequency
  - Matching our hearing

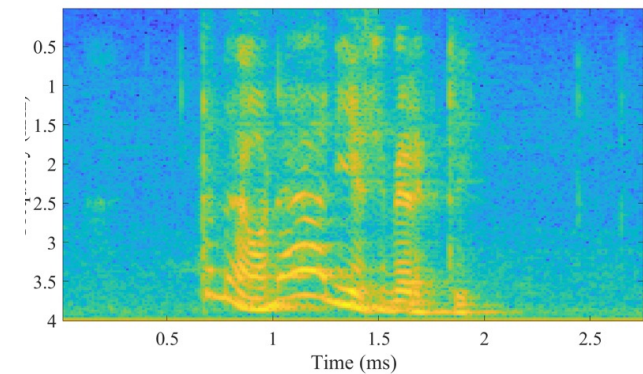
$$m = 2595 \log_{10} \left( 1 + \frac{f}{700} \right)$$



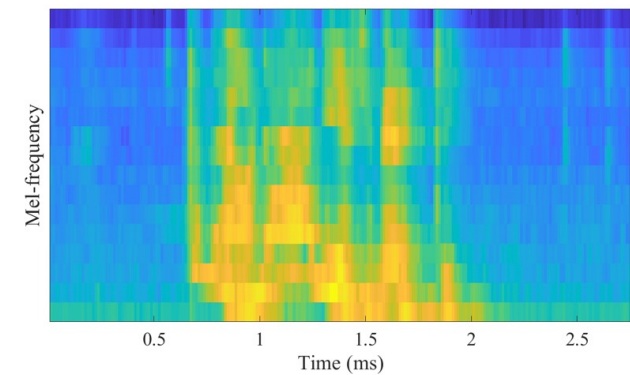
# Spectrogram to Mel Spectrogram

- Mel spectrograms use Mel Filter banks
  - Effectively bins for the frequency mapping
- Shape retained. Fine structure smoothed.

Spectrogram of a segment of speech



Spectrogram after multiplication with mel-weighted filterbank

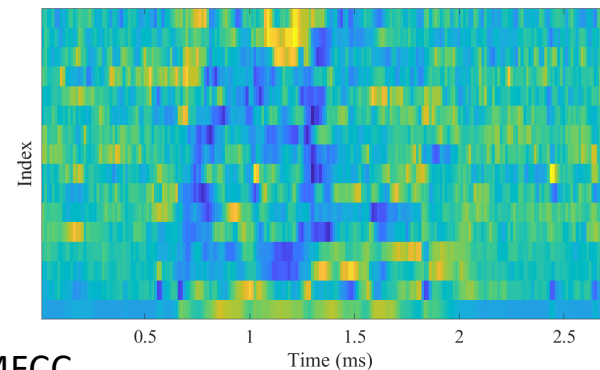




# Mel Frequency Cepstral Coefficients

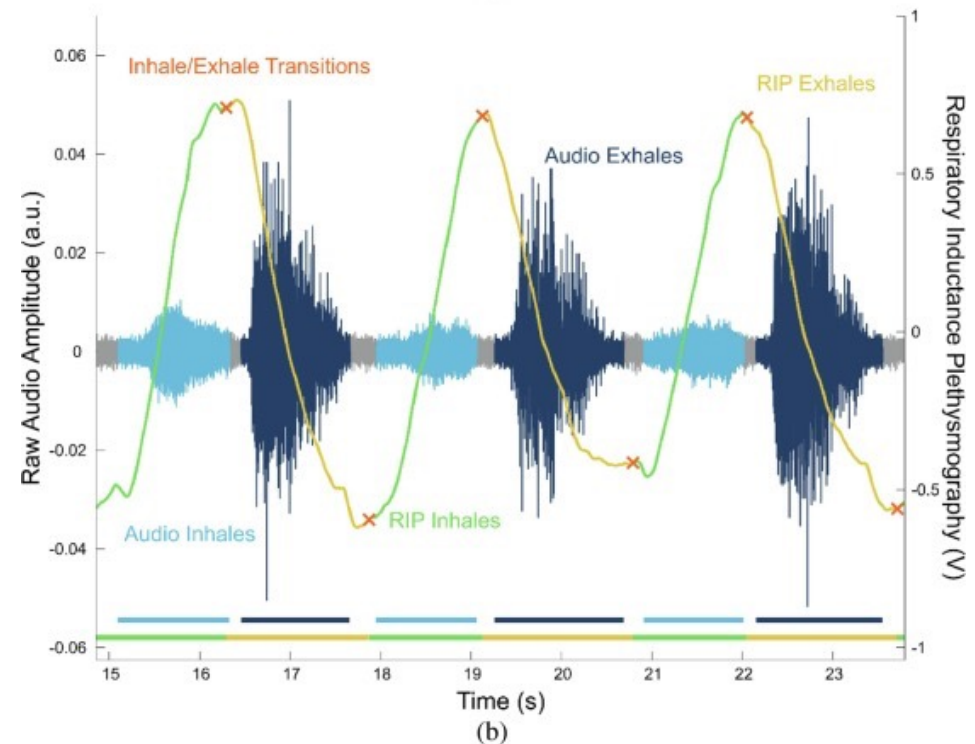
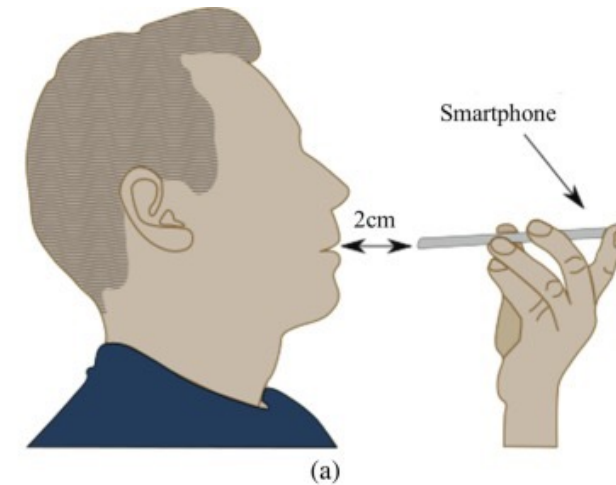
- Steps

- Apply a DFT to generate a frequency plot from time domain plot.
- Log the data and apply Mel Scaling.
- Discrete Cosine Transform (a transformation which highlights the important parts of the log DFT graph).
- Result is a number of “coefficients”: first 12-13 are the most relevant generally for audio.



# Respiratory Pattern Detection from Audio

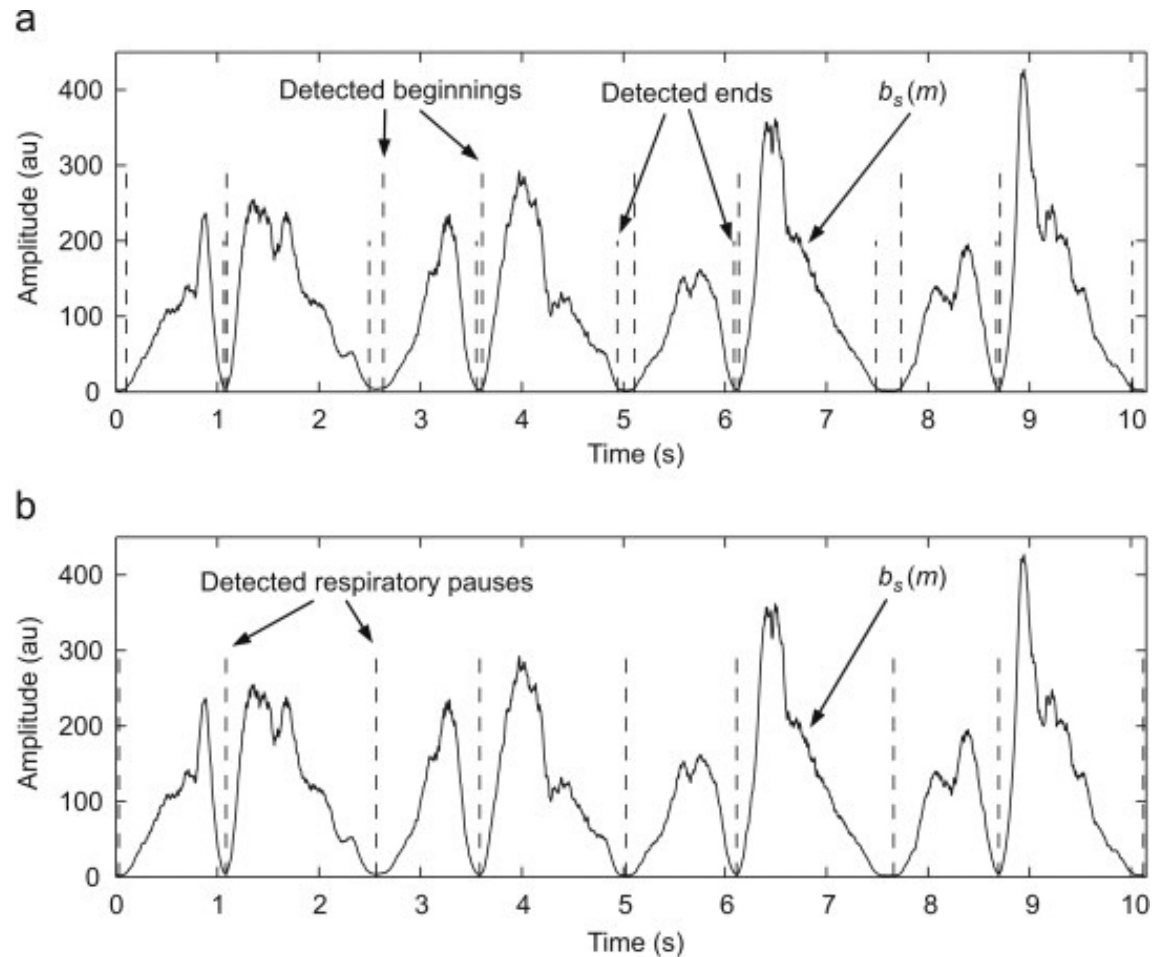
- Green/yellow line is ground truth data from chest strap.
- In-out breathing audio patterns can be visibly distinguished on time domain audio plot.



E Doheny, Ben P.F. O'Callaghan, Vitória S. Fahed, Jérémy Liegey, Cathy Goulding, Silke Ryan, Madeleine M. Lowery, Estimation of respiratory rate and exhale duration using audio signals recorded by smartphone microphones, Biomedical Signal Processing and Control, Volume 80, Part 1, 2023,

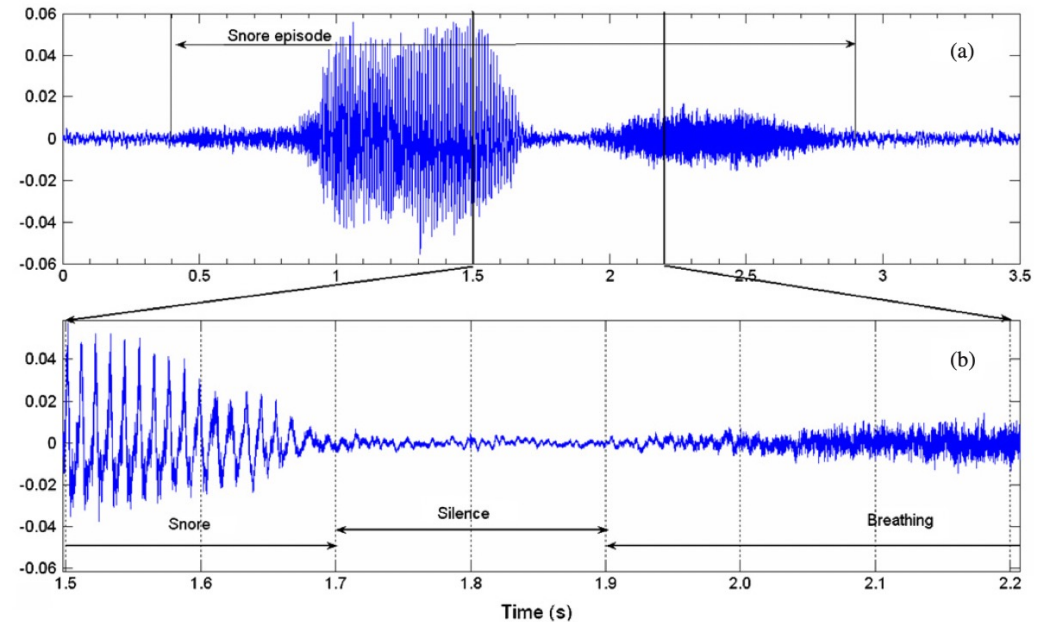
# Breathing Pattern Detection

- Signal passed with filters to isolate the right frequencies.
  - 8th order Butterworth low-pass filter with cut-off frequency of 1 kHz.
- Elimination of signal with coughs, yawning etc: windowing and max and median peak amplitude used.
- Time domain features used to detect pauses in respiration.

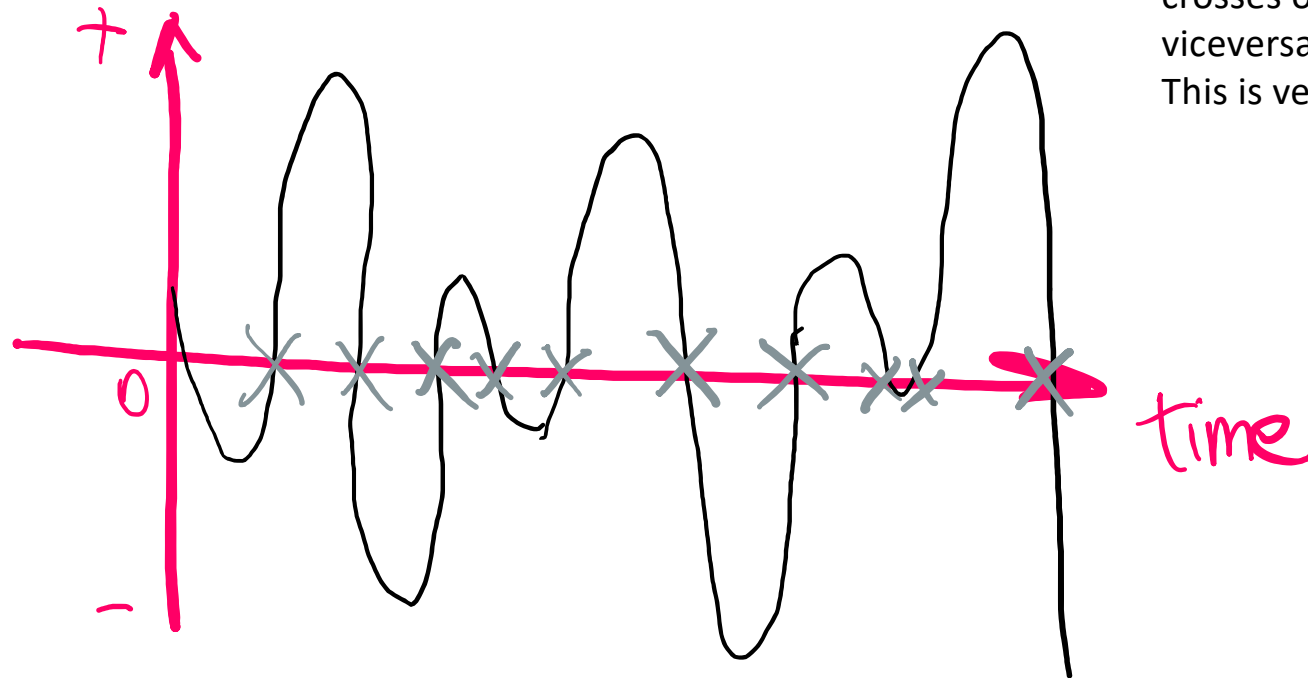


# Snoring-non Snoring

- Identification of voiced snoring, breathing and silence.
- Features
  - number of zero crossings in a given length of time
  - the energy of the signal
  - normalized autocorrelation coefficient at 1 ms delay
  - first predictor coefficient of linear predictive coding (LPC) analysis



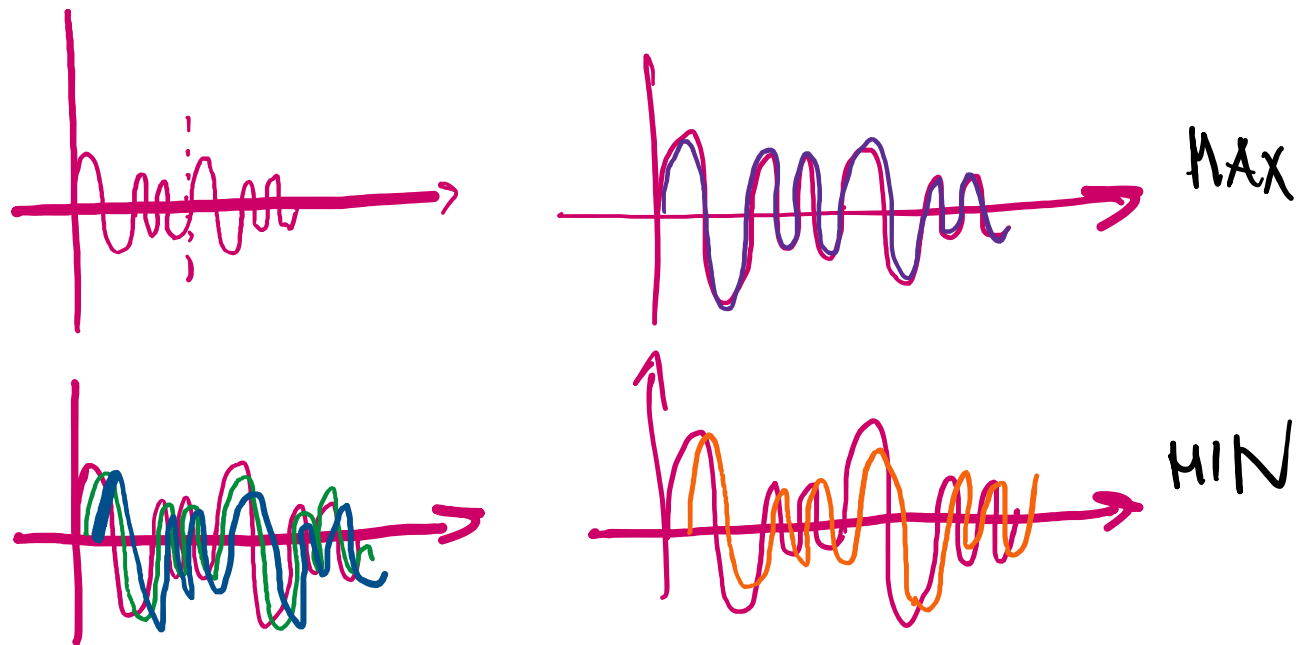
# Zero Crossing Rate



Measures the number of times a signal crosses over from positive to negative and viceversa (per time period).  
This is very correlated to frequency generally.

# Autocorrelation (useful to find period)

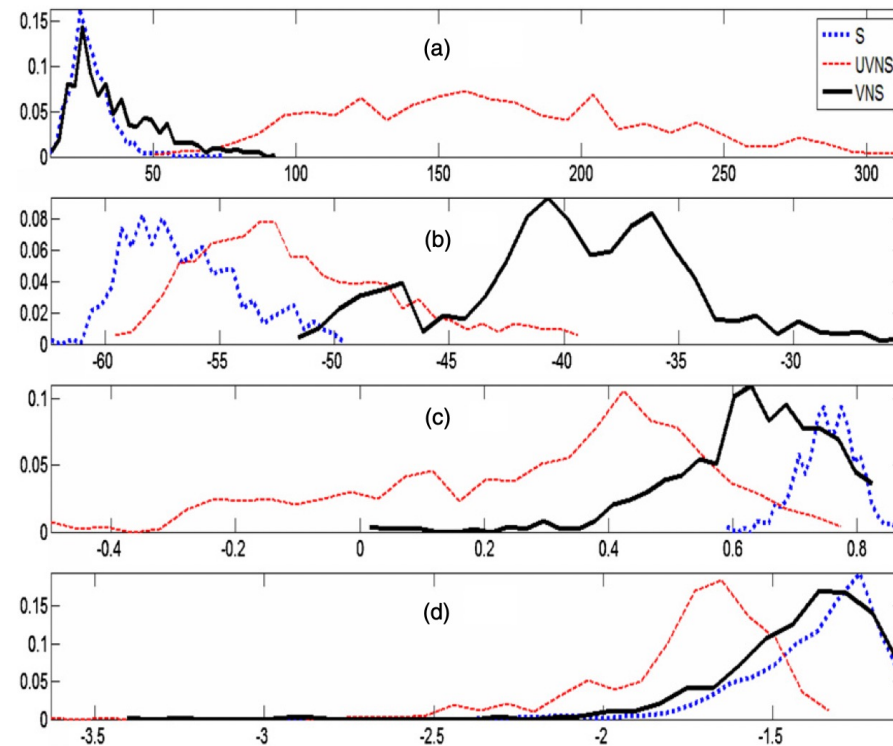
$$R(m) = \sum_{n=0}^{N-1-m} s(n)s(n+m)$$



# Performance: Probability distribution of the features for classification

PDF of  
-zero crossing  
-log of energy  
-autocorrelation coefficient  
-first linear predictor coefficient

S= silence  
UNS = Unvoiced non silence  
VNS = voiced non silence



# Sleep Apnea

Cessation of airflow to the lungs that lasts at least for 10s and is associated with at least 4% drop in blood's oxygen saturation level (SaO<sub>2</sub>).





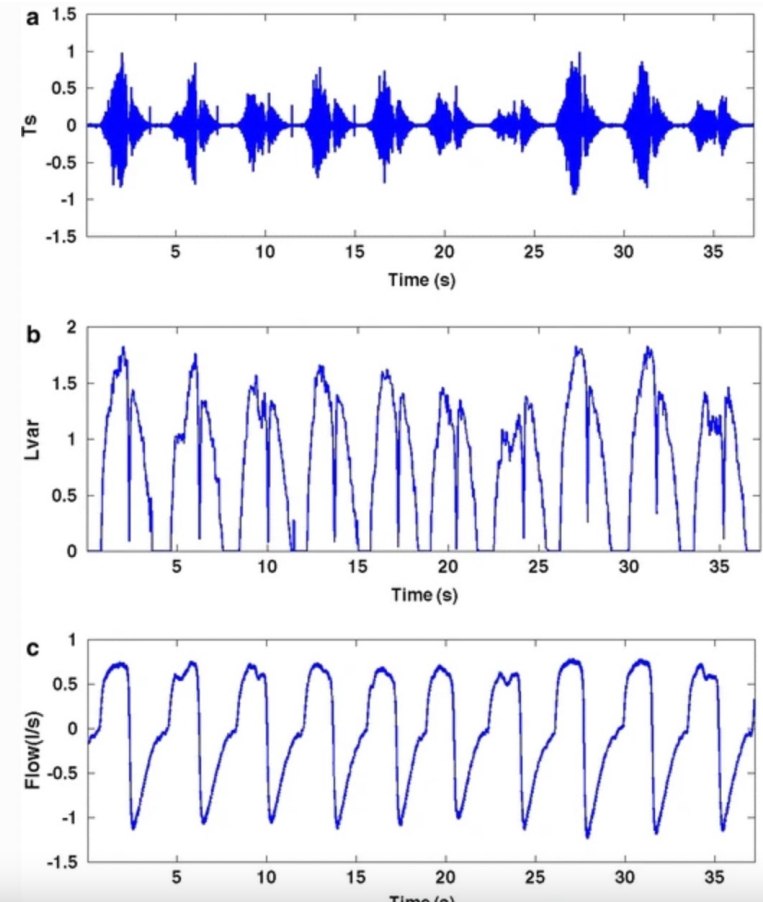
# Air Flow and Tracheal Sounds

**Log of energy** of the tracheal **sound signal** is a good indicator of **air flow**

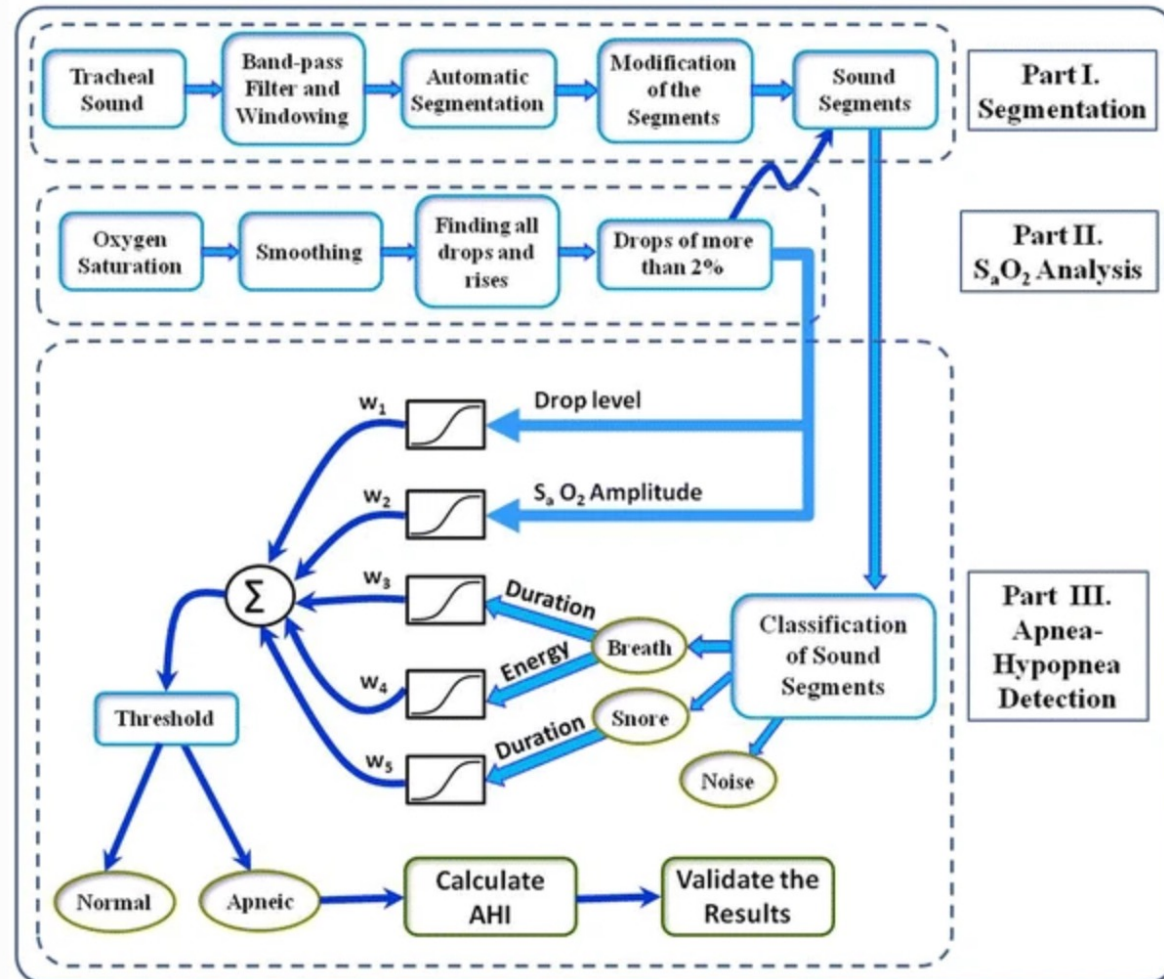
Signal

Log energy

True flow  
(measured with mask)

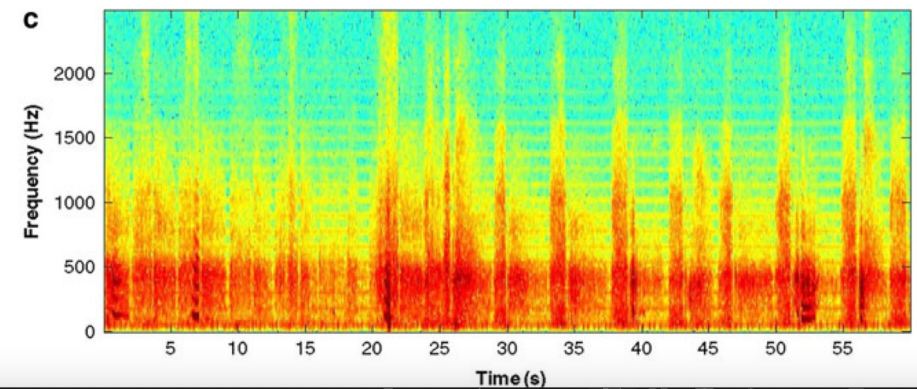
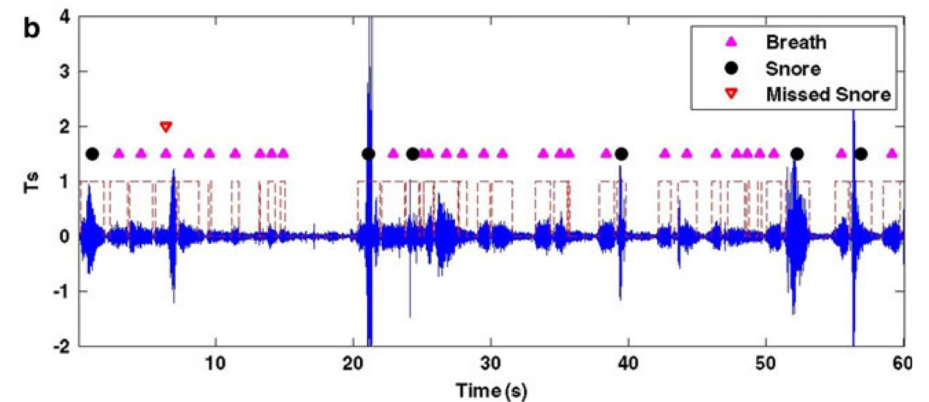


# Sleep Apnea Detection with Audio and SaO<sub>2</sub> monitoring



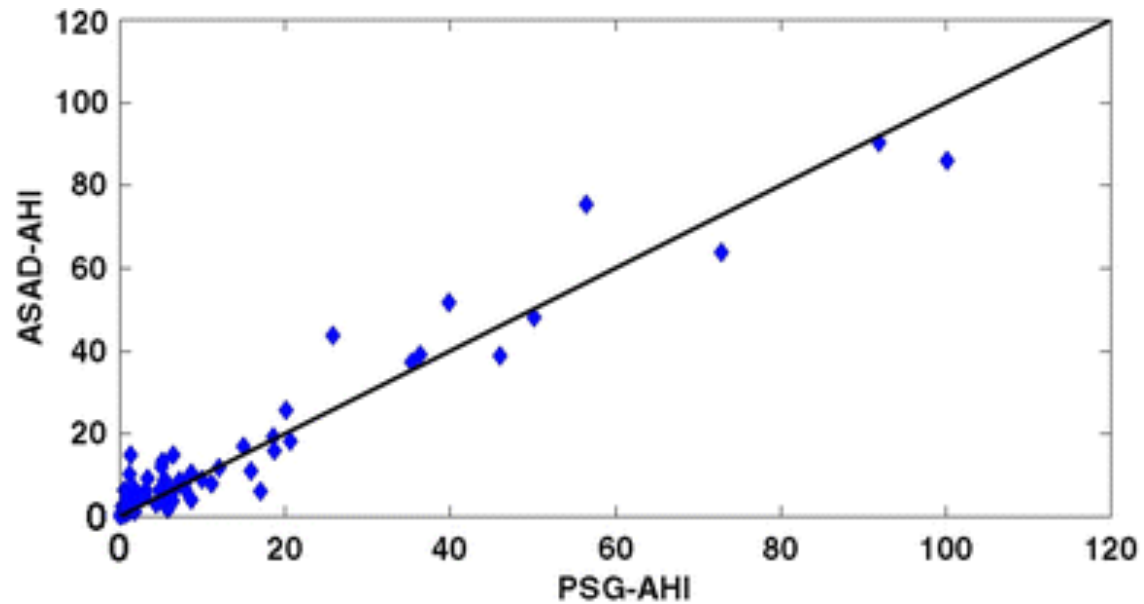
# Sleep Apnea Detection

- Classification of the sound in snore, breathing and noise
  - Use of energy and duration (a mixture)
- Spectrogram shows the snoring appearing in deep colours



# Results

- AHI: apnea–hypopnea index

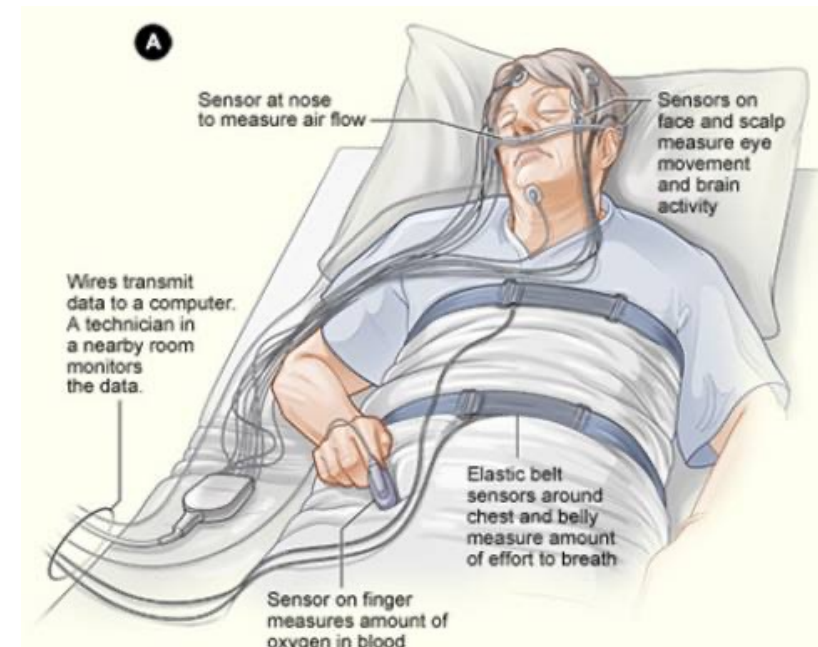


# Sleep Stages Classification with Audio

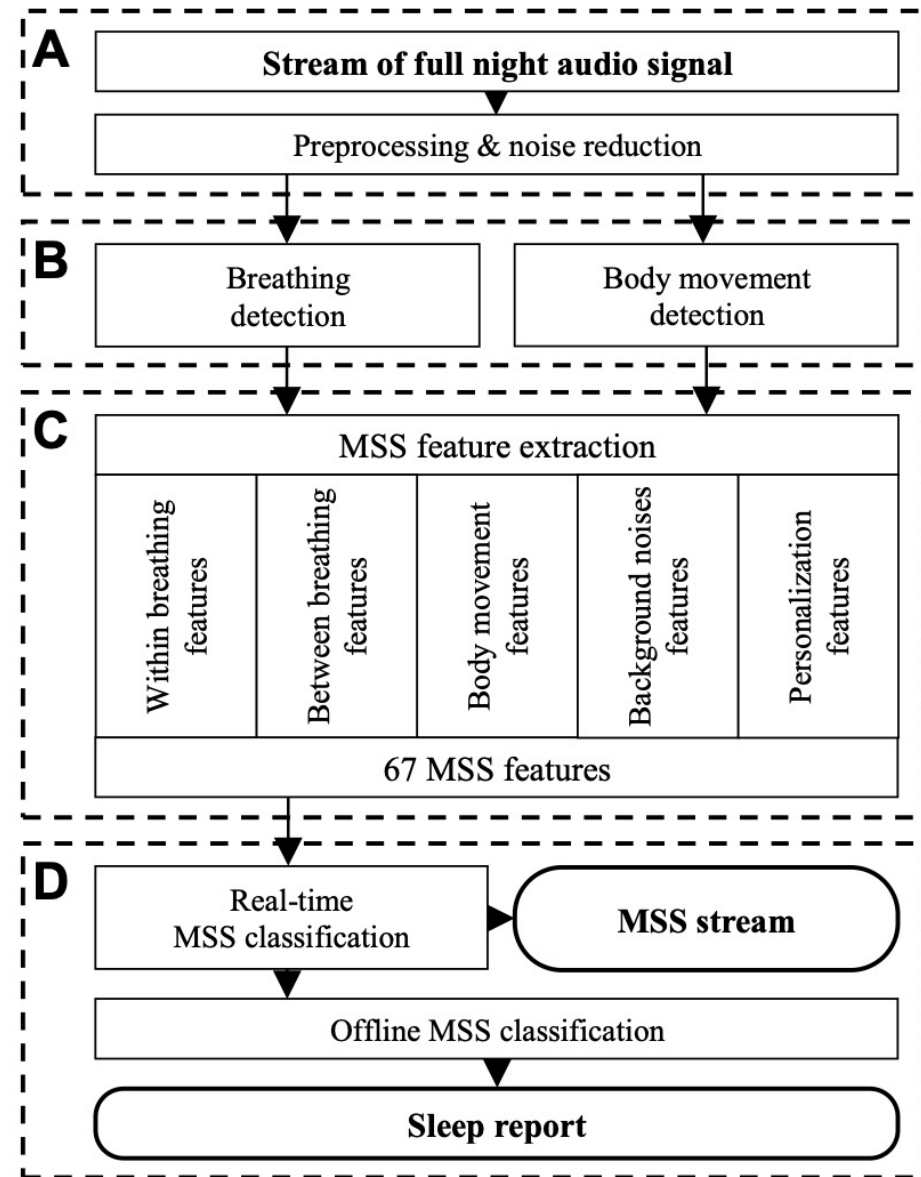
- During sleep (in contrast to wakefulness) there is an increase of upper airway resistance due to decreased activity of the pharyngeal dilator muscles, which is reflected **by amplification of air-pressure oscillations during breathing**. These air-pressure oscillations are perceived as breathing sounds during sleep.
- REM (rapid-eye movement), N(on)REM, and wakefulness are associated with lack of, some, and considerable body movement.
- Breathing pattern is more periodic and consistent in deep NREM sleep compared to REM and wakefulness

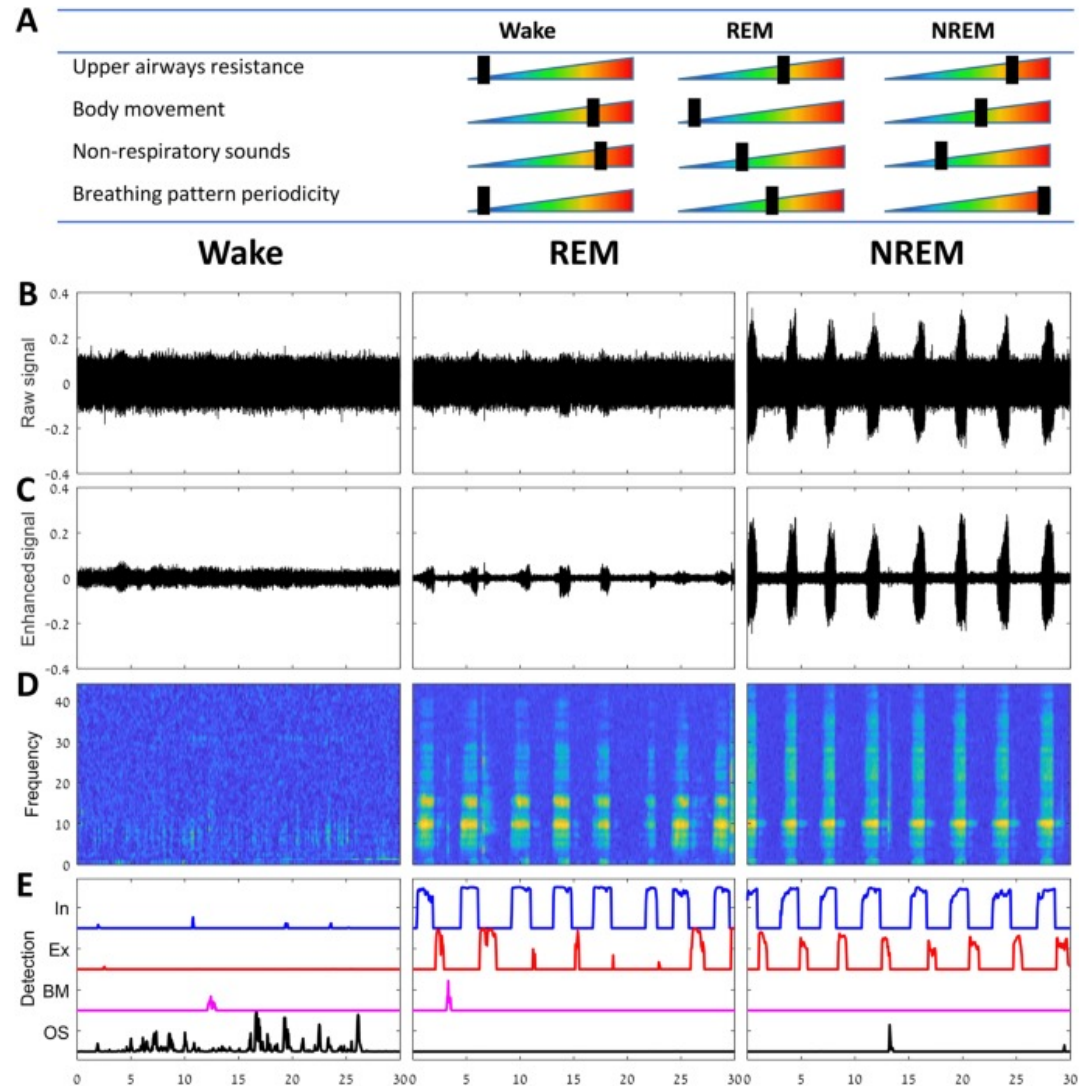
# Audio

- Microphone on the bed: (Edirol R-4 pro, Bellingham, WA, USA) with a directional microphone (RØDE, NTG-1, Silverwater, NSW, Australia) was placed at a distance of one meter above the subject's head and used for acquiring the audio signals.
- Polisomnography (PSG) for ground truth



# Detection of Macro Sleep Stages (MSS)





Raw sound

Preprocessed

Spectrogram

Inhalation (blue), Exhalation (red), body movement (pink) and other (black)



# Within Breathing Features

- During sleep, airways resistance is higher than during wakefulness, hence breathing efforts become greater, which translates into several factors including **louder breathing** sounds, prolonged **breathing duration**, and **different vocal sounds** (snores).

		count	importance
<b>A.</b>	<b>Within breathing features (WB)</b>	<b>33</b>	<b>0.270</b>
	Detection score of inspiration ( $\mu, \sigma$ )	2	0.093
	Detection score of expiration ( $\mu, \sigma$ )	2	0.048
	Detection score of respiration ( $\mu, \sigma$ )	2	0.037
	Duration inspiration ( $\mu, \sigma$ )	2	0.075
	Duration expiration ( $\mu, \sigma$ )	2	0.024
	Stationarity inspiration ( $\mu, \sigma$ )	2	0.013
	Stationarity expiration ( $\mu, \sigma$ )	2	0.009
	Sound intensity inspiration ( $\mu, \sigma$ )	2	0.044
	Sound intensity expiration ( $\mu, \sigma$ )	2	0.009
	Sound intensity inspiration top 1% ( $\mu, \sigma$ )	2	0.027
	Sound intensity expiration top 1% ( $\mu, \sigma$ )	2	0.053
	Entropy inspiration ( $\mu, \sigma$ )	2	0.045
	Entropy expiration ( $\mu, \sigma$ )	2	0.008
	Frequency centroid inspiration ( $\mu, \sigma$ )	2	0.031
	Frequency centroid expiration ( $\mu, \sigma$ )	2	0.036
	Frequency bandwidth (resp., insp., expi.)	3	0.009

# Between Breathing Features

- Alternations in ventilation may affect fundamental respiration factors such as respiratory cycle period, respiratory duty cycle, and respiration consistency, and can be measured using sound analysis. These respiration factors are most likely to have more substantial variability during REM as opposed to NREM.

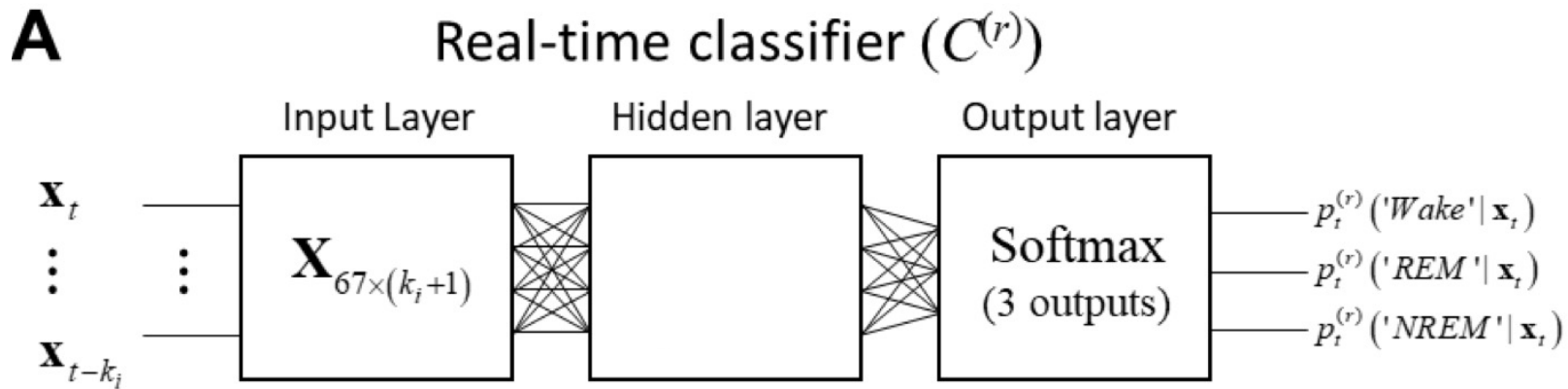
<b>B. Between breathing features (BB)</b>		<b>12</b>	<b>0.267</b>
Respiration duty cycle	BB_DCR	1	0.026
Inspiration duty cycle	BB_DCI	1	0.058
Expiration duty cycle	BB_DCE	1	0.020
Respiration cycle period ( $\mu, \sigma$ )	BB_RCP	2	0.033
Respiration cycle period consistency	BB_RCPC	1	0.068
Respiration cycle periods fourth-order curve	BB_RCPfit	5	0.023
Breathing Count	BB_BC	1	0.006

# Body Movement Features

- Wakefulness is accompanied by relatively greater body movement, compared to NREM, while during REM sleep body movement should be absent by definition.

<b>C. Body movement features (BM)</b>		<b>10</b>	<b>0.054</b>
Body movement average score	BM_AS	1	0.002
Body movement overall score percentiles	BM_OS	7	0.017
Sound intensity body movement (all curve)	BM_SI	1	0.007
Sound intensity body movement 10% (all curve)	BM_SI01	1	0.038

# Real time Classification



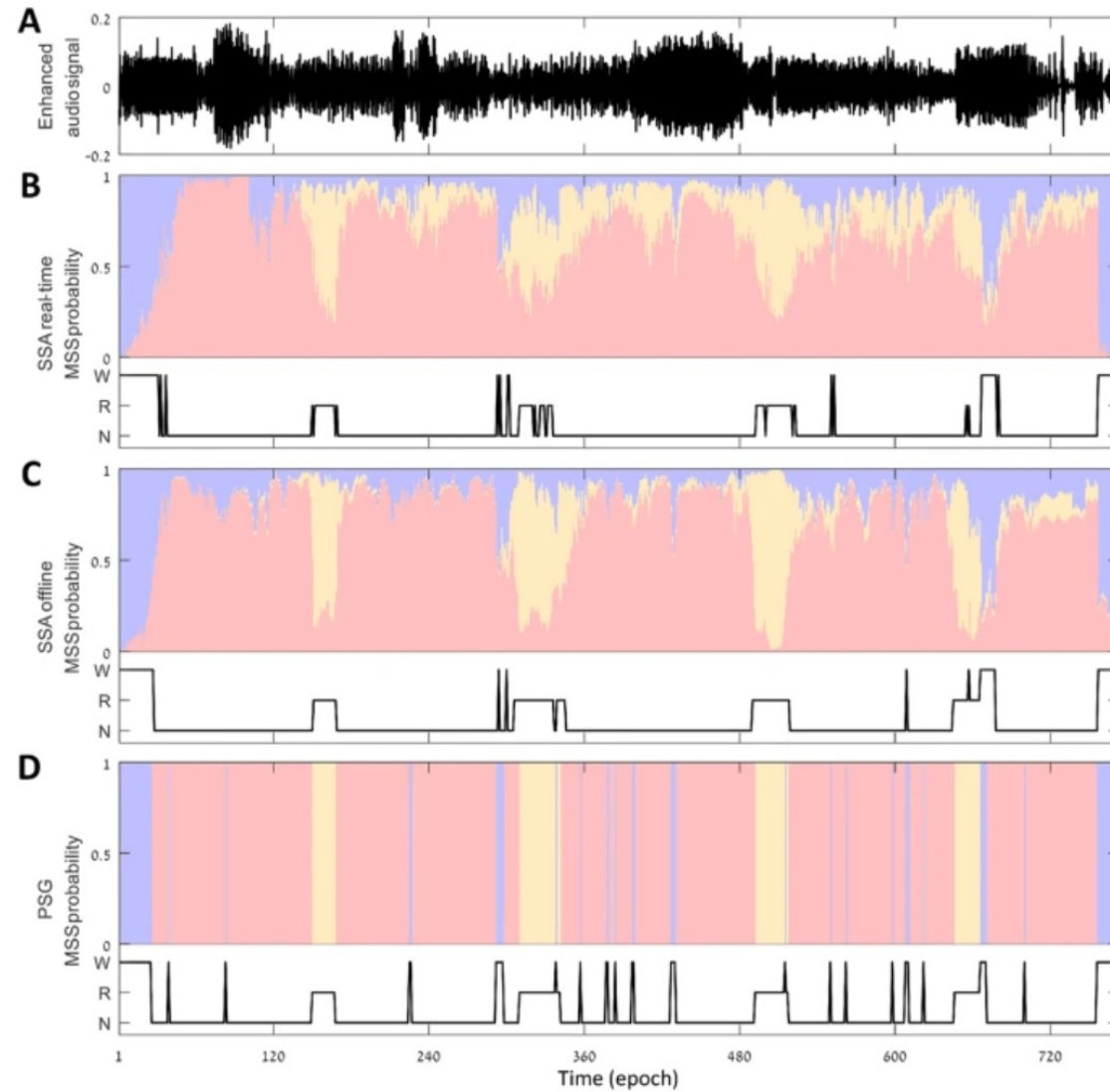
# Results

One Subject

Blue= wake

Orange= REM sleep

Red= Non-REM sleep



# Questions